

# Monitoring of Cerebral Blood Flow

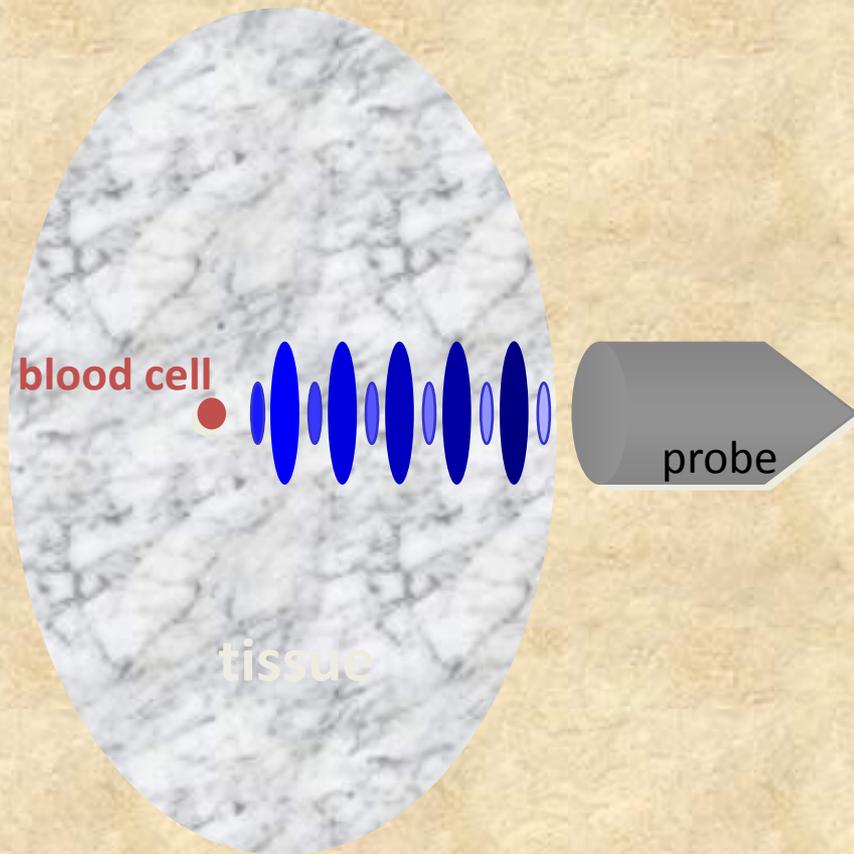
**Transcranial Doppler**

**Laser Doppler Flowmetry**

**Thermal dilution method (Hemedex)**



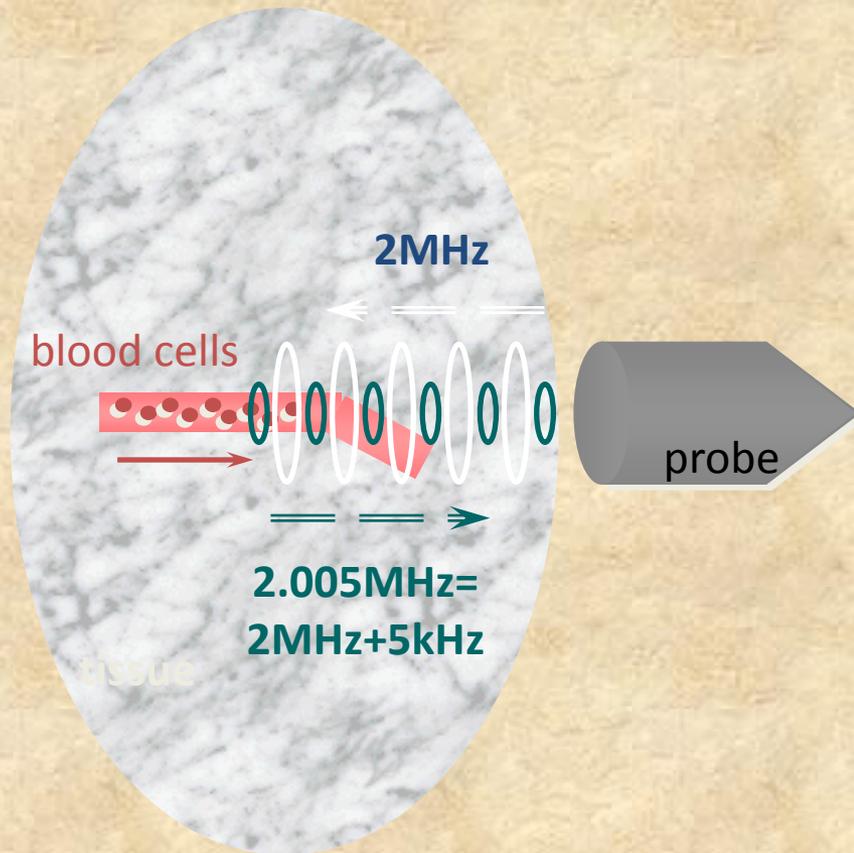
# *Ultrasound in Tissue*



## Some Facts:

- ultrasound travels at a constant speed of 1540m/s in tissue.
- ultrasound is reflected at the boundary of two media.
- ultrasound is backscattered in heterogenous tissues.
- the higher the ultrasound frequency the higher the attenuation and the hollower the penetration depth.

# Doppler Principle in Sonography



- ❑ a ultrasound signal is used to insonate the vessels, e.g. 2MHz.
- ❑ this signal is reflected and backscattered from moving objects (e.g. blood cells) with a positive or negative frequency shift.
- ❑ the frequency shift is also called Doppler shift or Doppler signal.
- ❑ the faster the blood cells are moving the higher Doppler shift.



# Doppler Formula

Doppler Frequency Shift:

$$f_d = \frac{2 * f_t * v * \cos \beta}{v_0}$$

Velocity:

$$v = \frac{v_0 * f_d}{2 * f_t * \cos \beta}$$

simplified:

$$v = f_d * \frac{1540 \text{m/s}}{2 * 2 \text{MHz} * 1}$$

$f_d$ : Doppler frequency shift

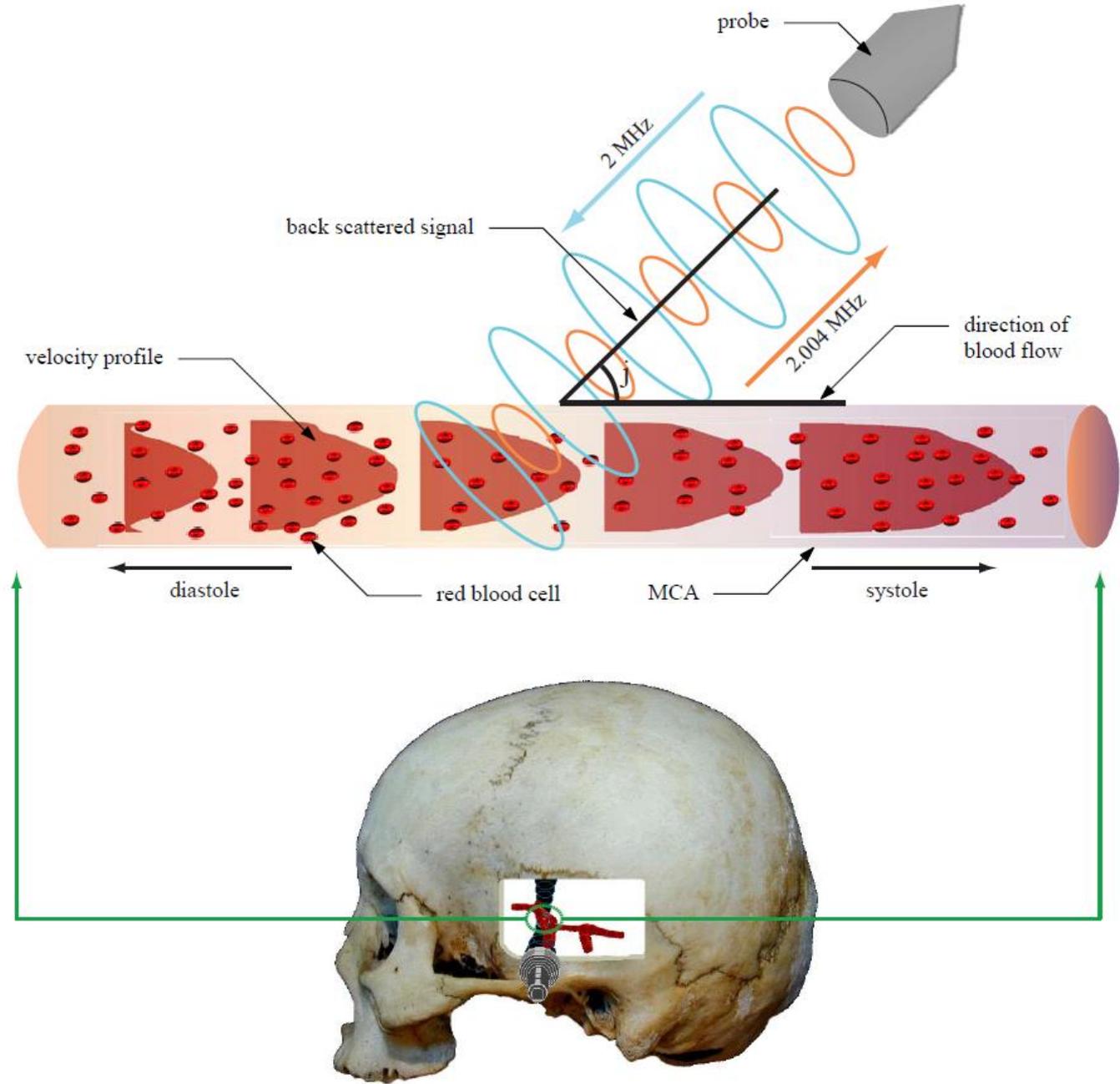
$f_t$ : ultrasound frequency, e.g. 2MHz

$v$ : velocity of the moving blood cells

$v_0$ : velocity of ultrasound in tissue (1540m/s)

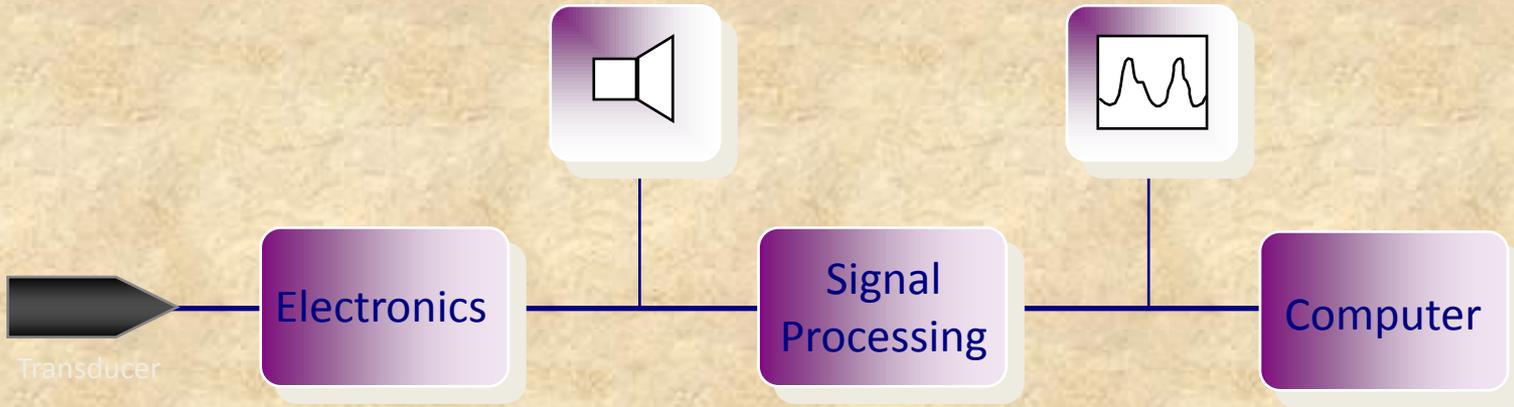
$\beta$ : angle of insonation

The Doppler frequency shift is the only variable in the above shown formula, therefore we have a linear relationship between blood flow velocity and Doppler frequency shift.



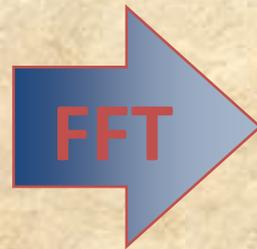
Thanks to Dr.DJ Kim

# Doppler System



## Audio Doppler Signal:

- Doppler signal
- time signal
- audio output
- difficult to analyze

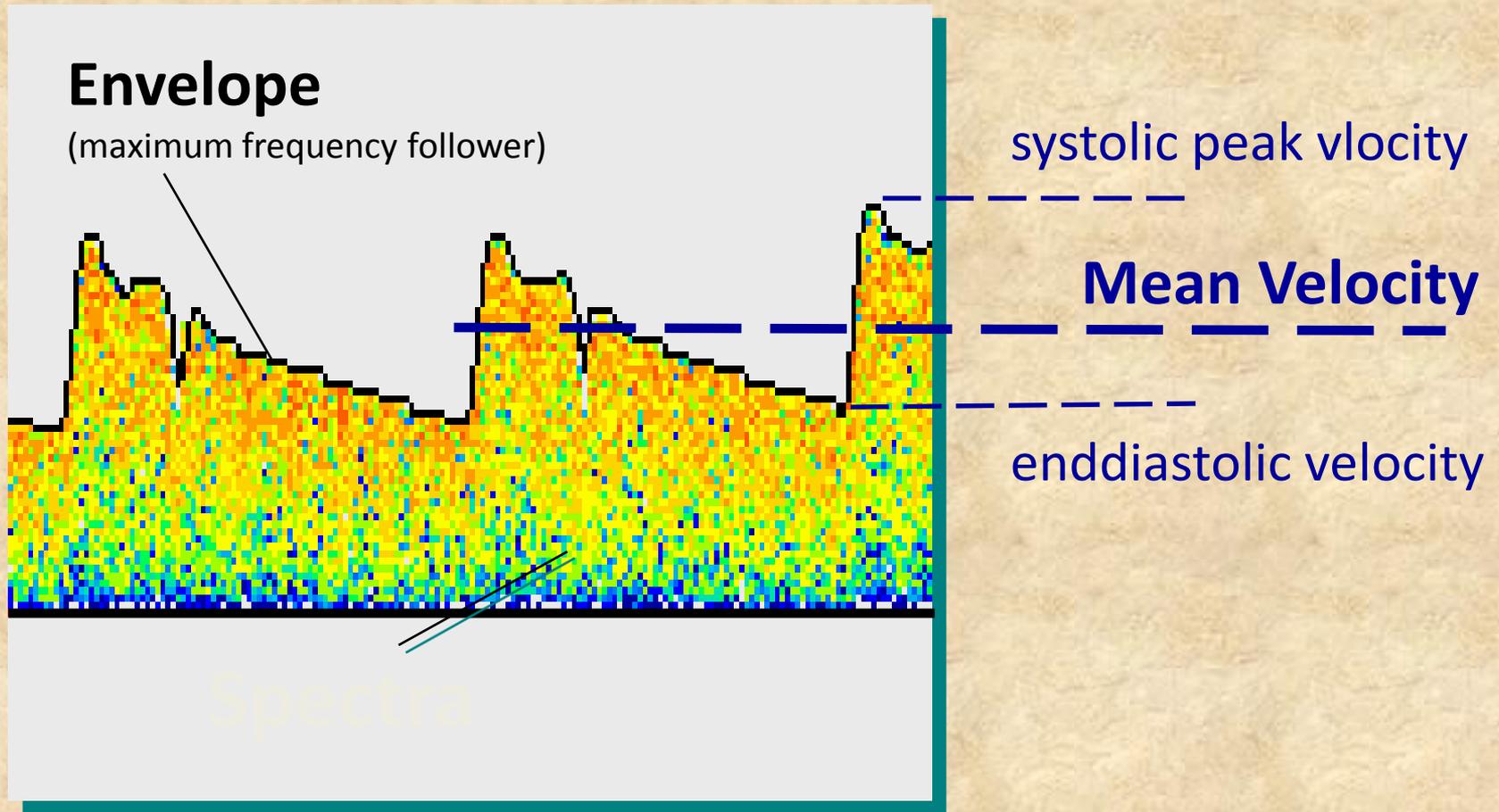


**Fast  
Fourier  
Transform**

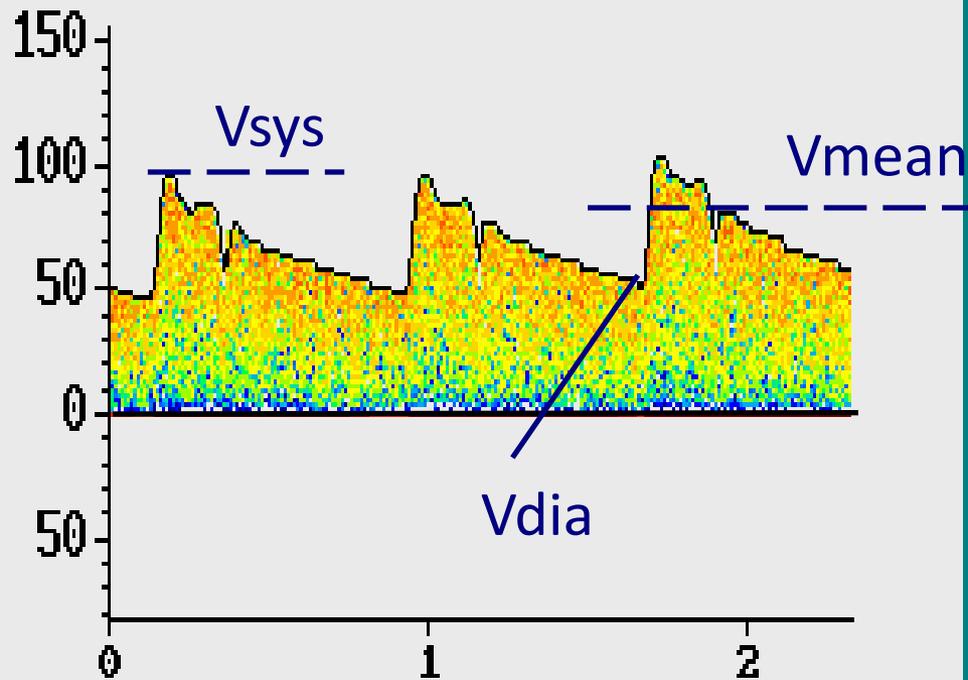
## Spectral Display:

- frequencies and velocities
- spectral display
- parameters like envelope, PI
- easier to analyze

# Spectral Display, Indices



# Pulsatility Indices



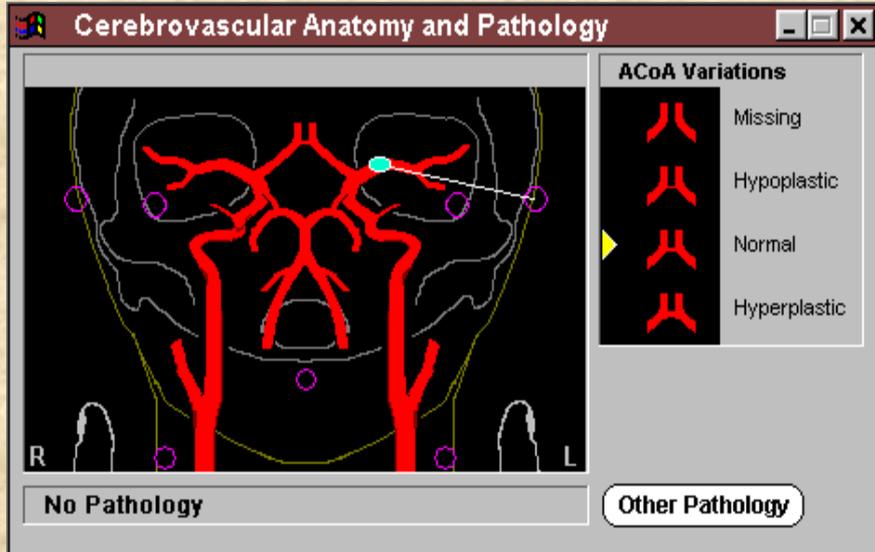
Gosling's Pulsatility Index

$$PI = \frac{V_{sys} - V_{dia}}{V_{mean}}$$

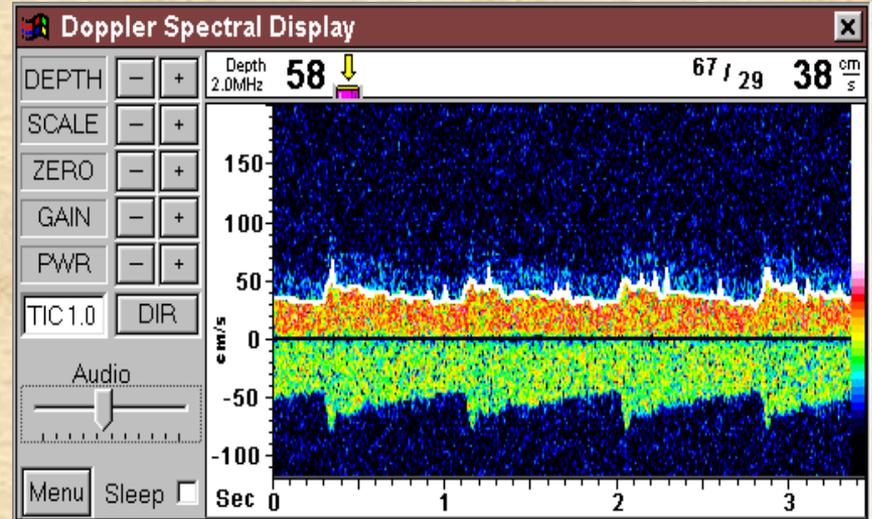
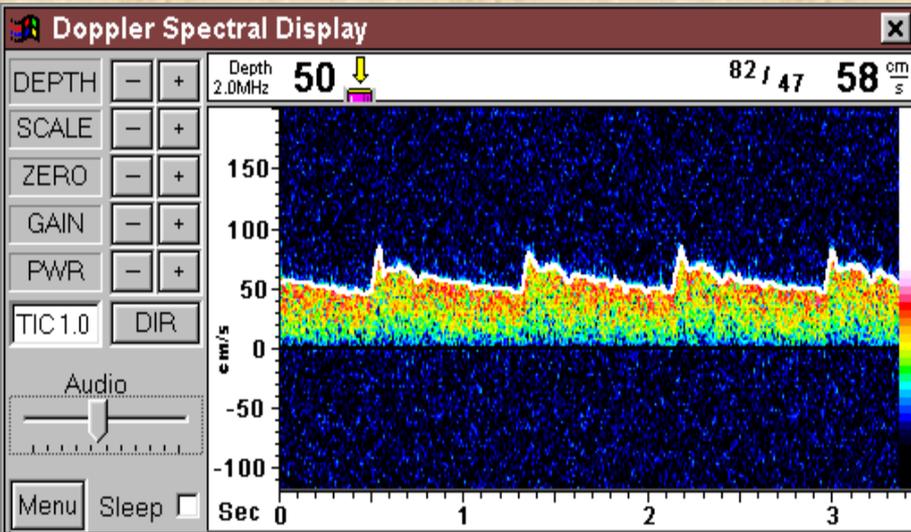
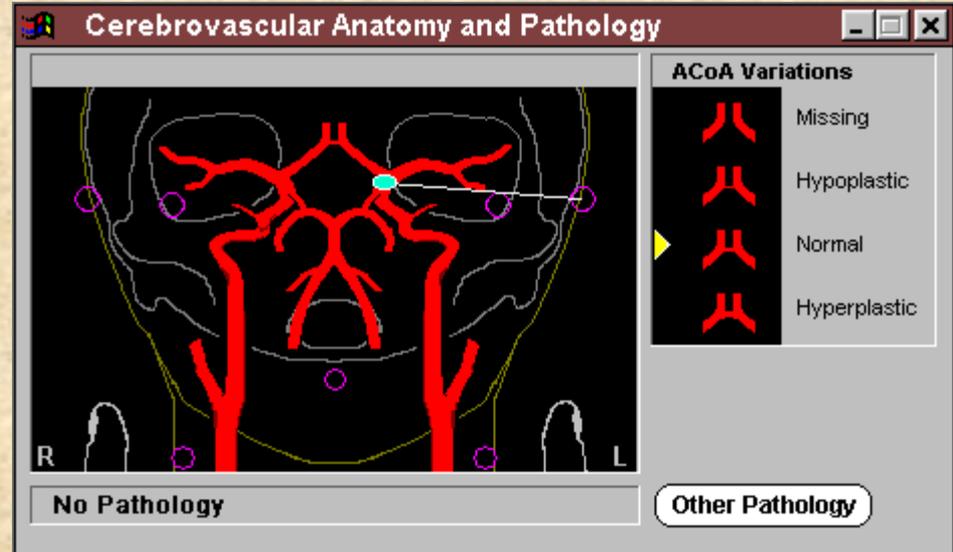
Pourcelot's Resistance Index

$$RI = \frac{V_{sys} - V_{dia}}{V_{sys}}$$

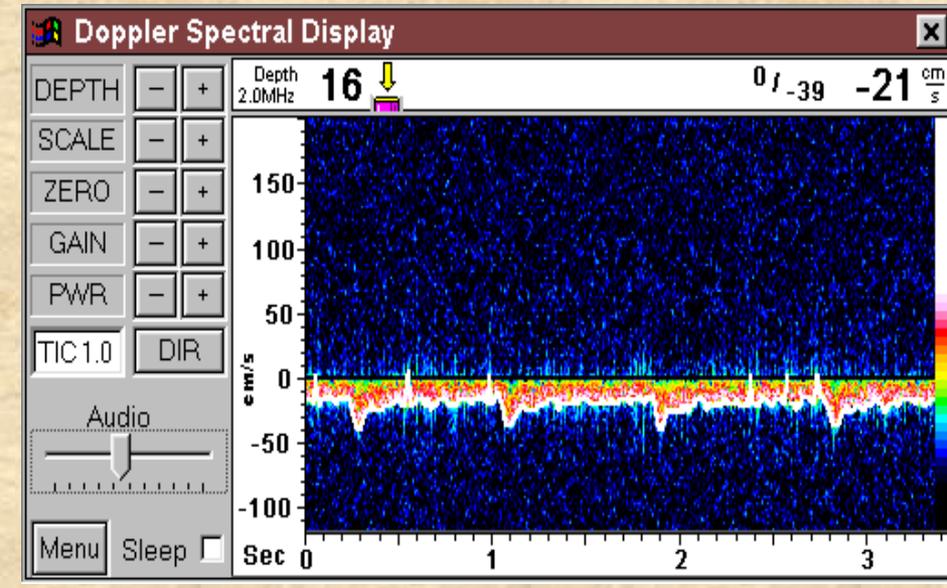
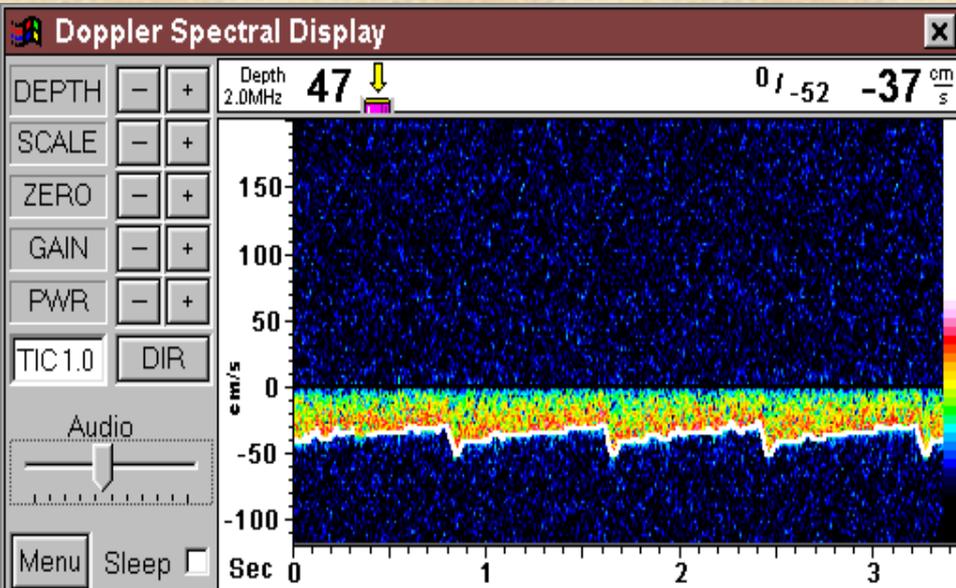
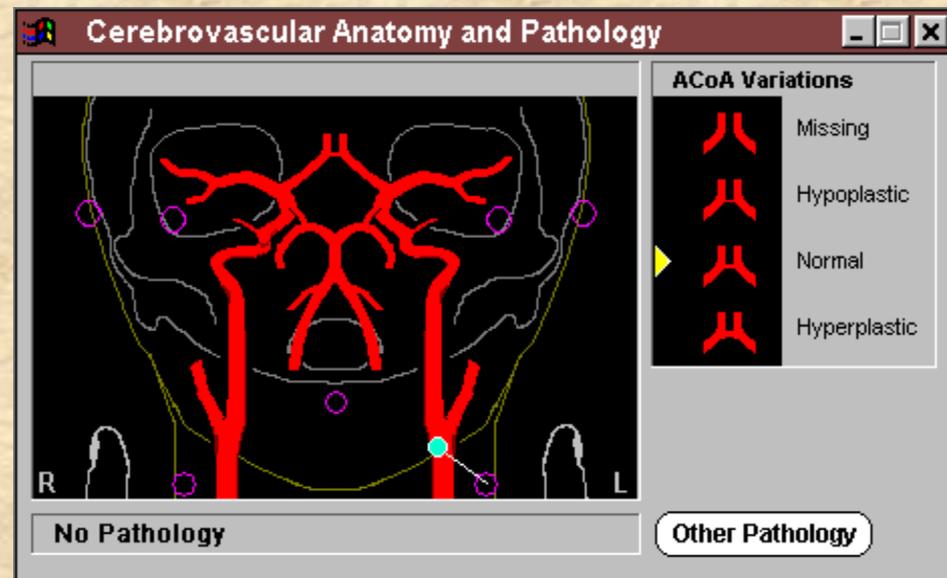
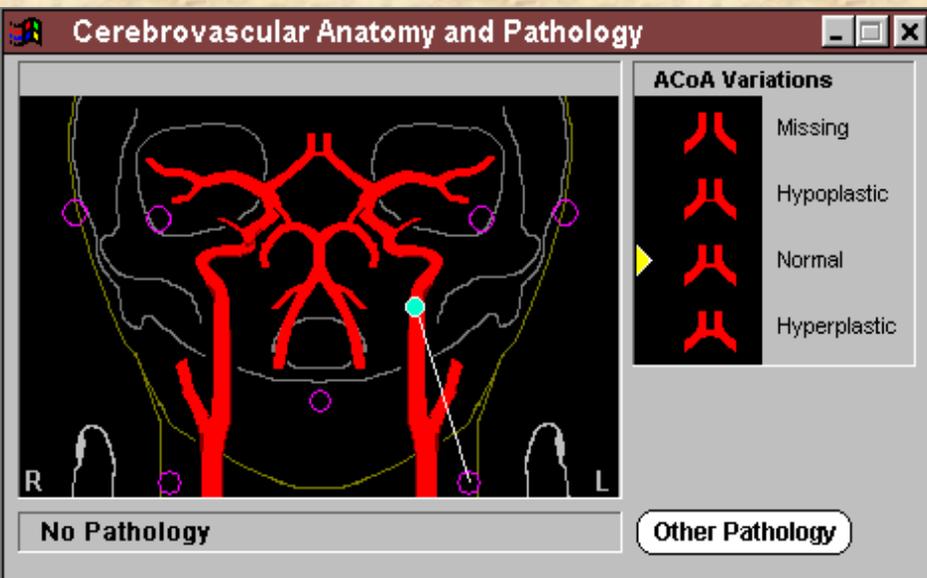
# MCA



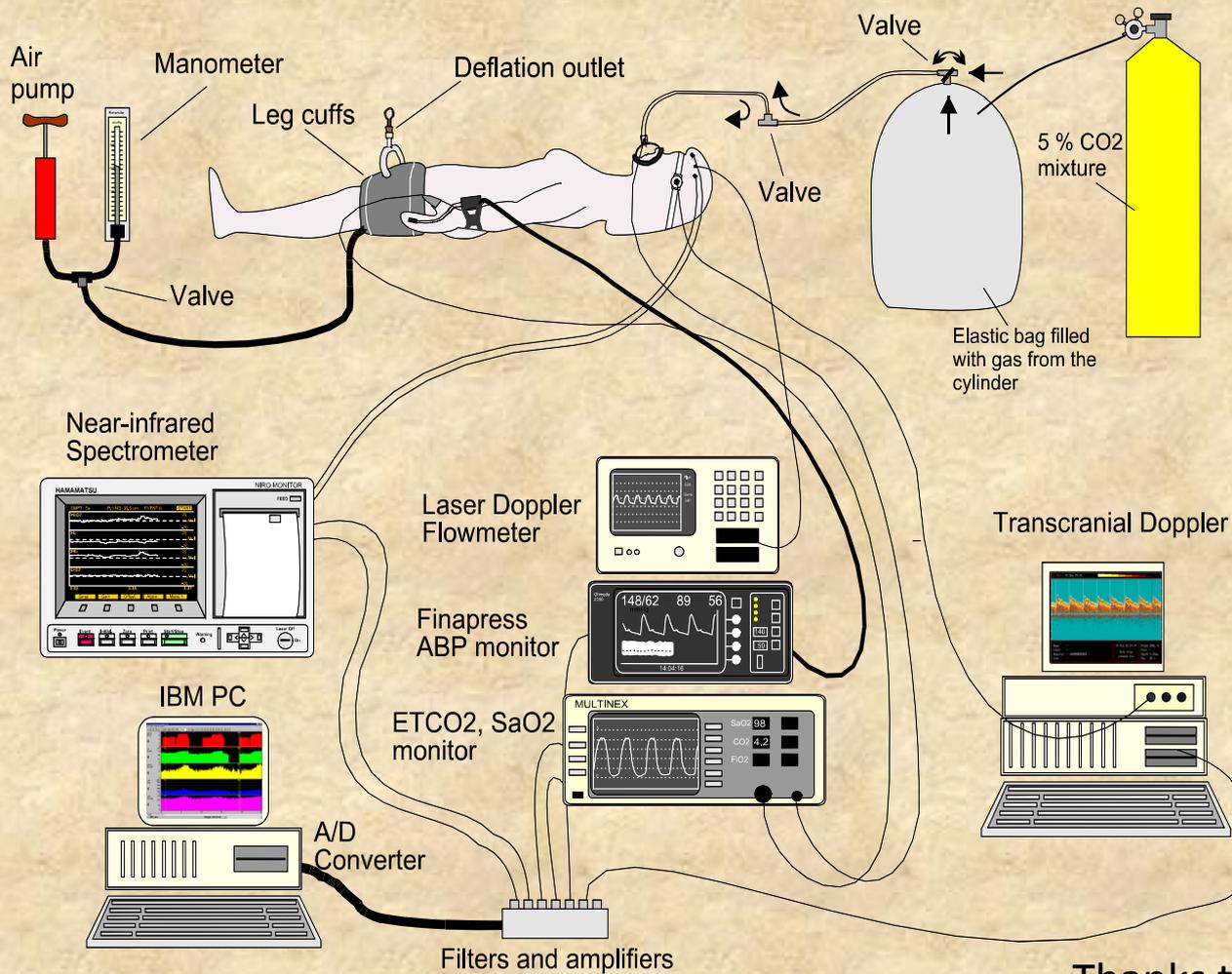
# Bifurcation



# Investigation of ICA



# Cerebrovascular Laboratory



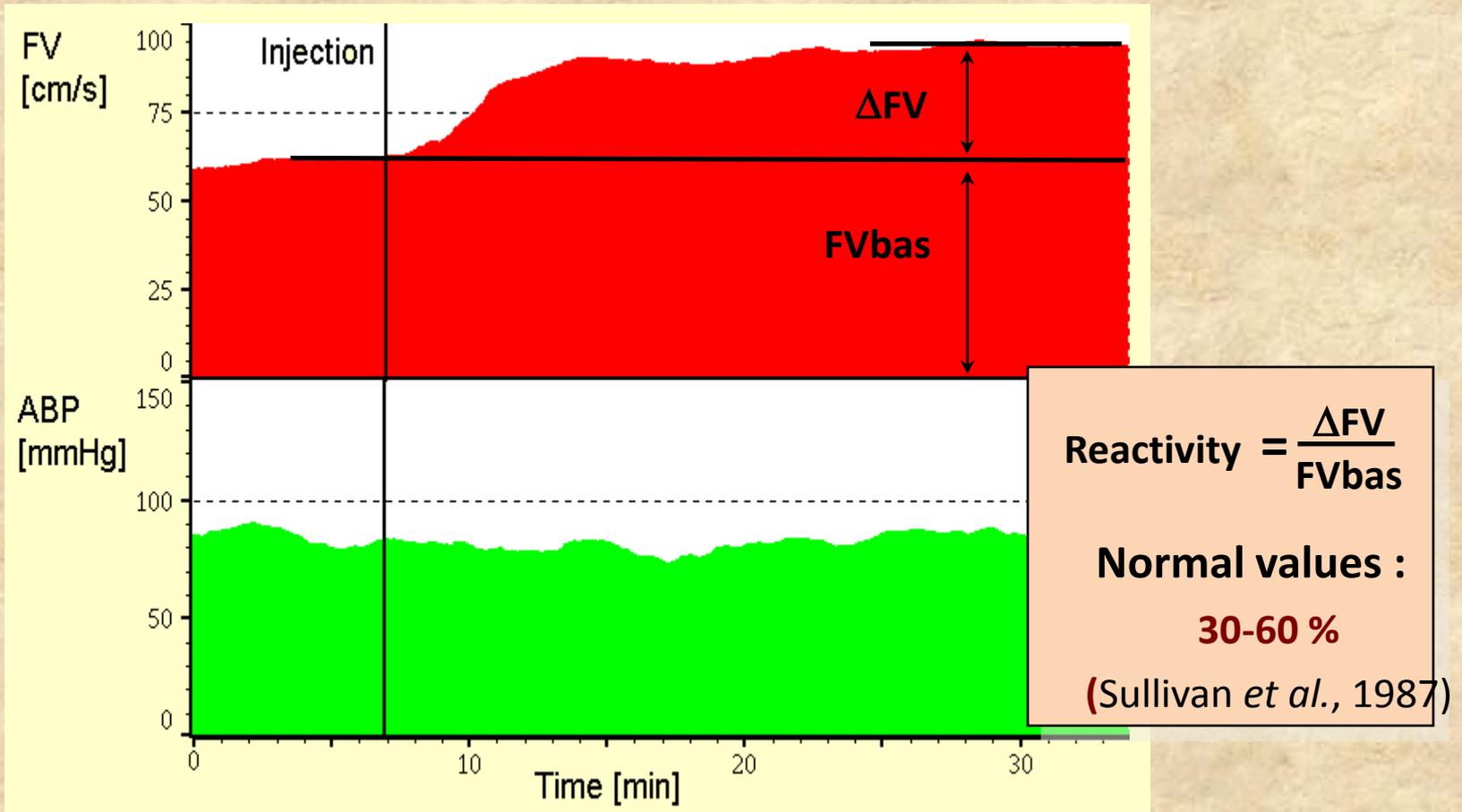
Thanks to Dr.P.Smielwski

# Testing of Cerebrovascular Reactivity using TCD

## Acetazolamide test

- Inhibitor of carbonic anhydrase in red cells.
- Intravenous administration of 1 g of acetazolamide causes normally 30%-60% increase in CBF.
- Advantages:
  - does not change ABP,
  - does not require patient's co-operation.
- Disadvantages: 2-h duration of action.

# Acetazolamide test

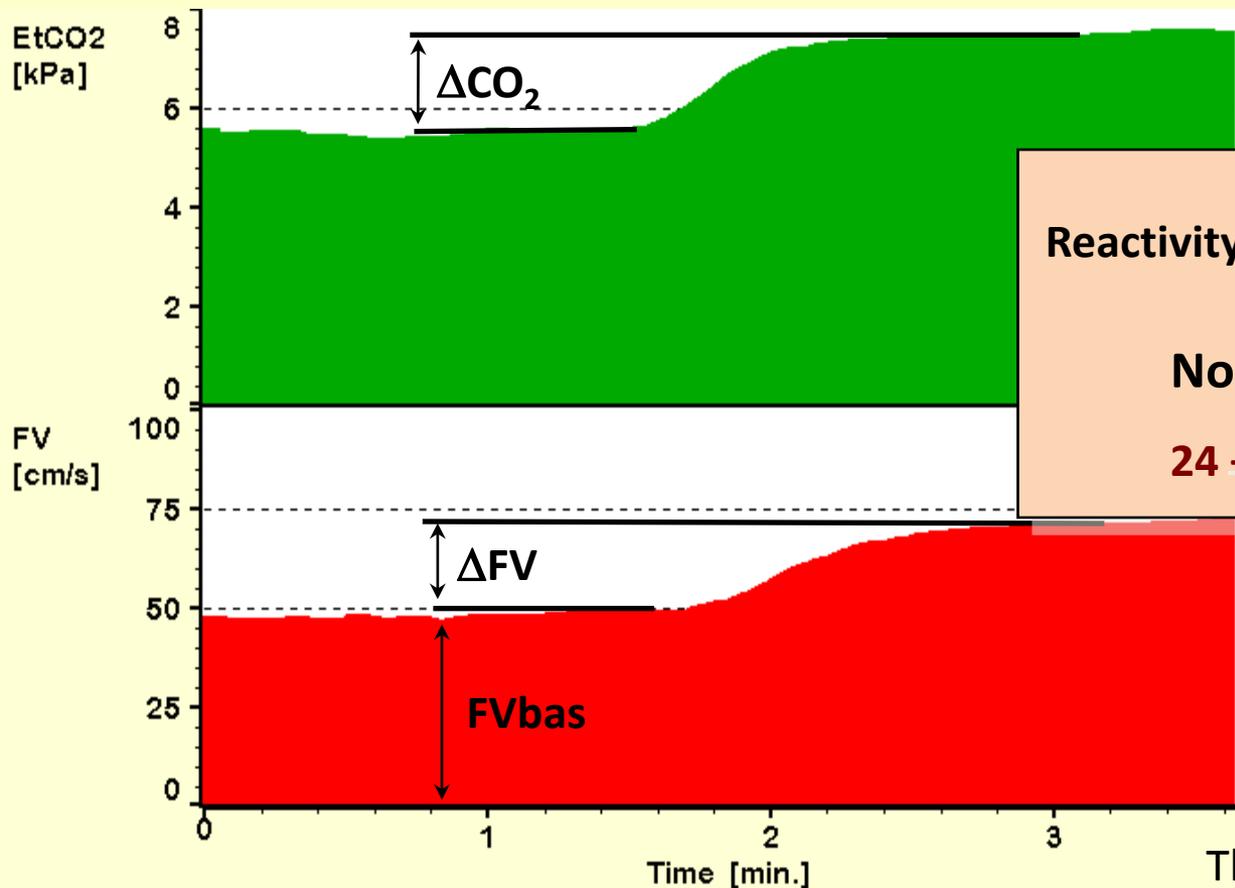


# CO<sub>2</sub> reactivity test

- Change in CO<sub>2</sub> concentration of the inspired gas
- Breath holding
- Manipulation of ventilation in sedated patients

# CO<sub>2</sub> Reactivity Methods of assessment

Change in FV to change in PaCO<sub>2</sub> ratio



$$\text{Reactivity} = \frac{\Delta\text{FV}}{\Delta\text{CO}_2} \cdot \frac{1}{\text{FVbas}}$$

Normal values :

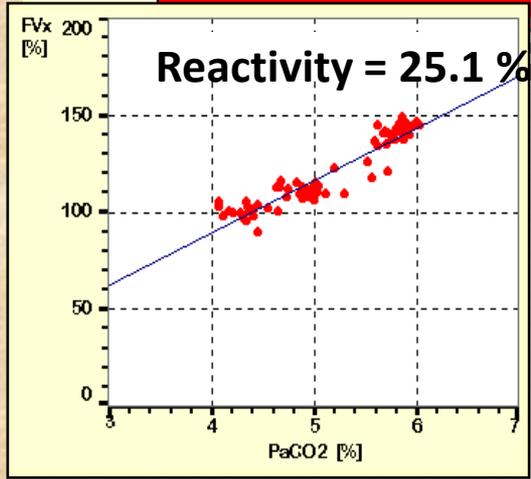
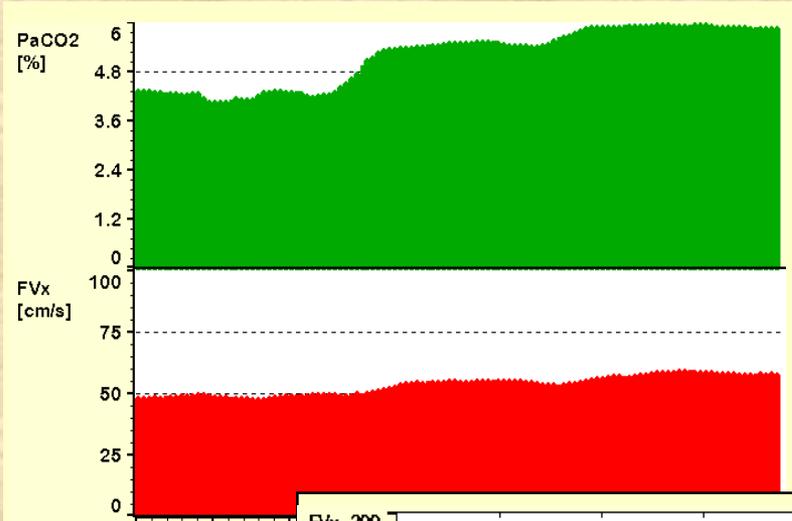
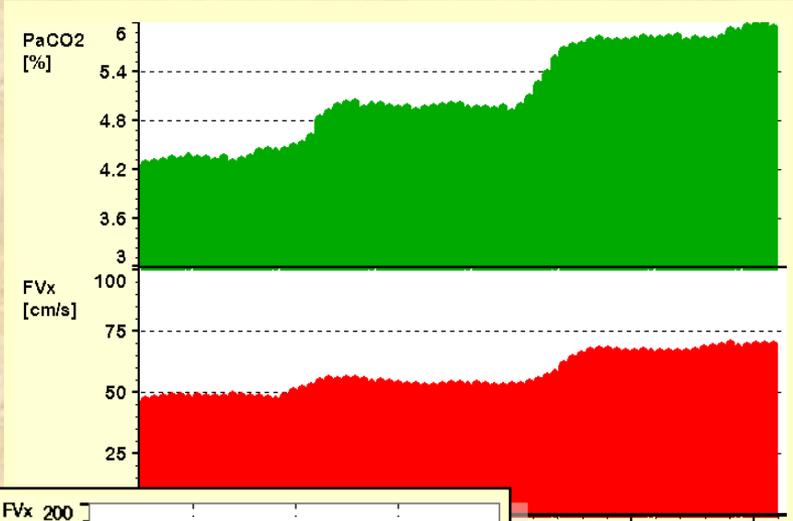
24 + 4.1 %/kPa

Thanks to Dr.P.Smielwski

Thanks to Dr.P.Smielwski

# CO<sub>2</sub> Reactivity Methods of assessment

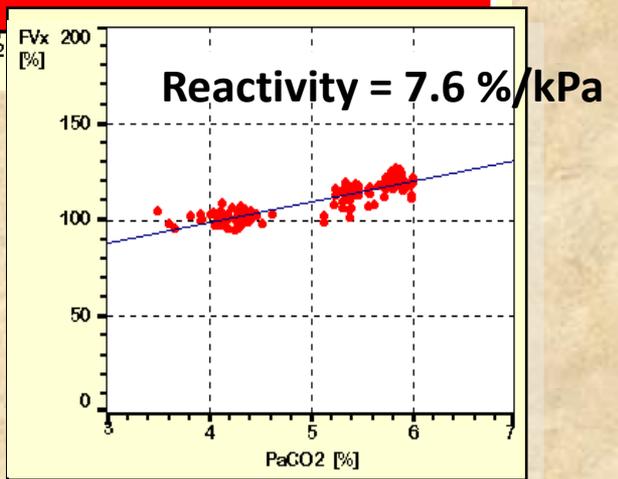
## Linear regression



**Reactivity = Slope of regr.**

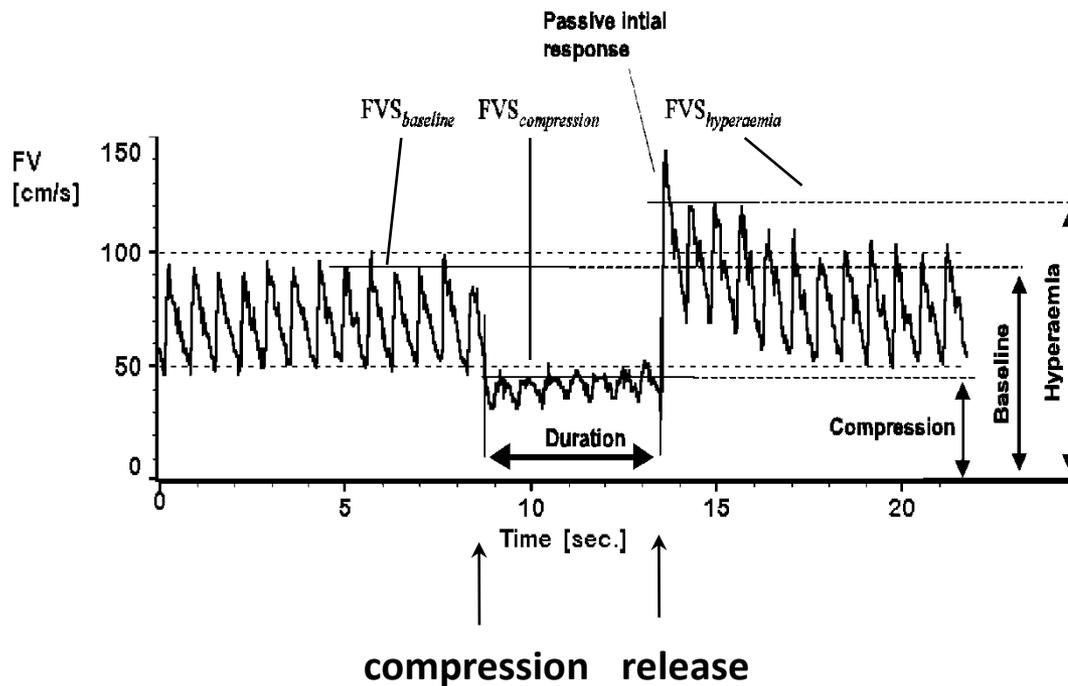
**Normal values :**

**24 + 4.1 %/kPa**



# Transient Hyperaemic Response Test Definition

Carotid compression

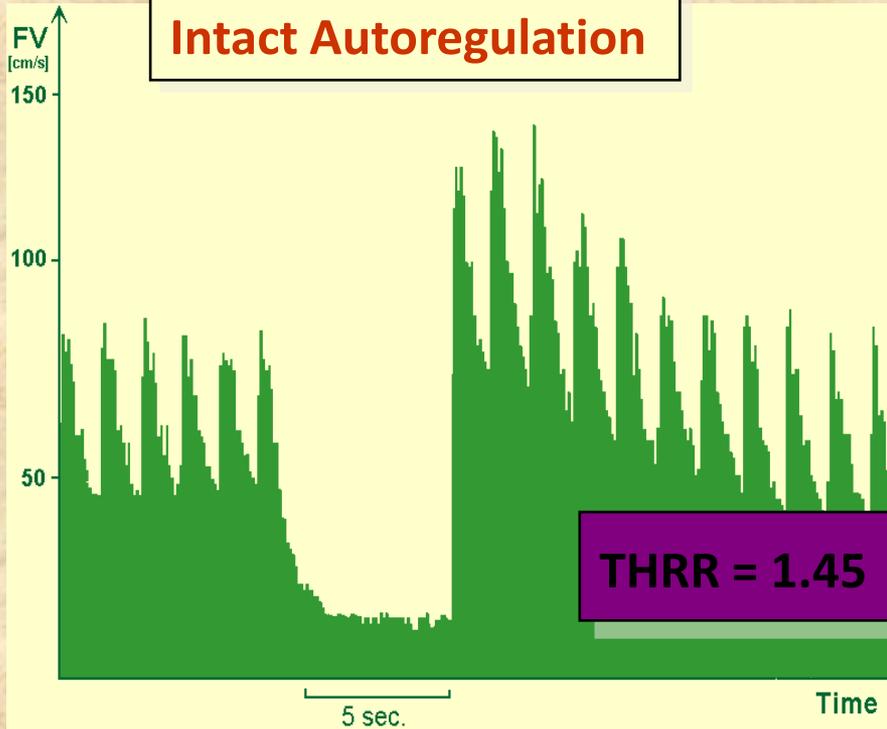


Transient hyperaemic response ratio

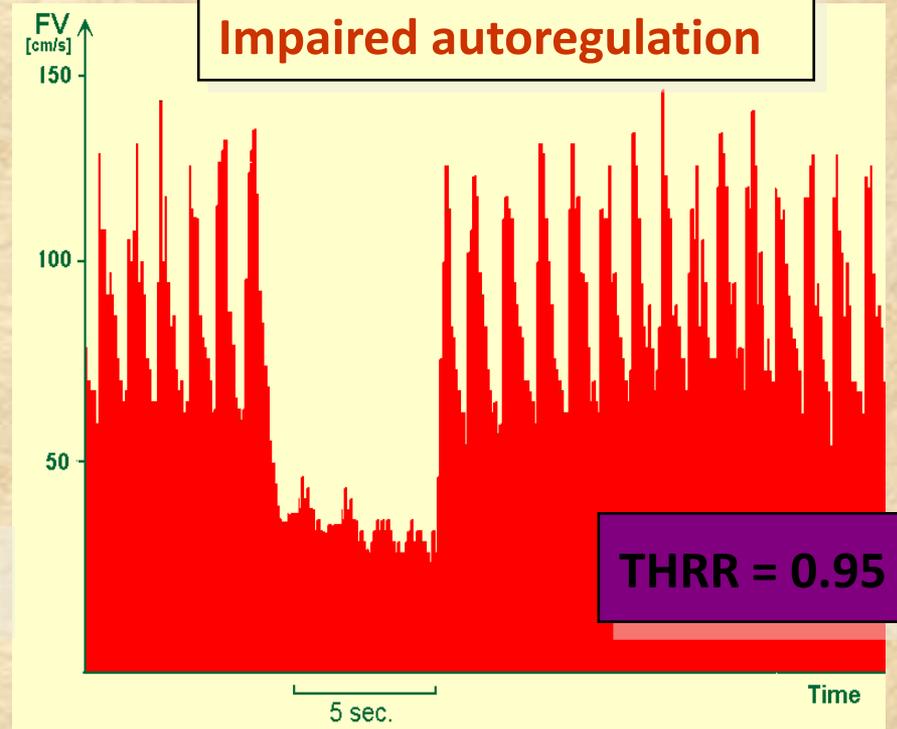
$$THRR = \frac{FVS_{hyperaemia}}{FVS_{baseline}}$$

# Transient Hyperaemic Response Test

**THRT Positive**  
Intact Autoregulation

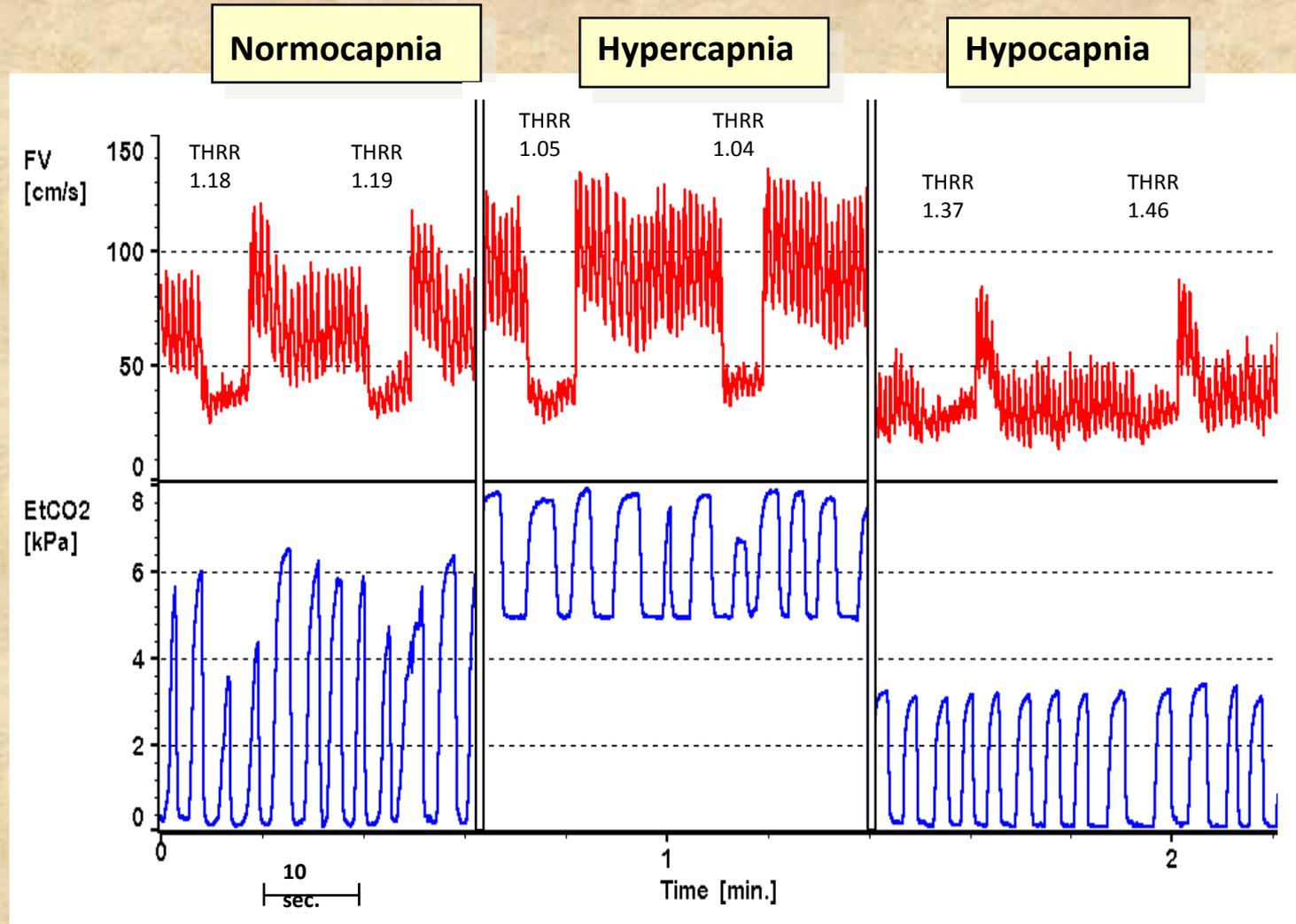


**THRT Negative**  
Impaired autoregulation



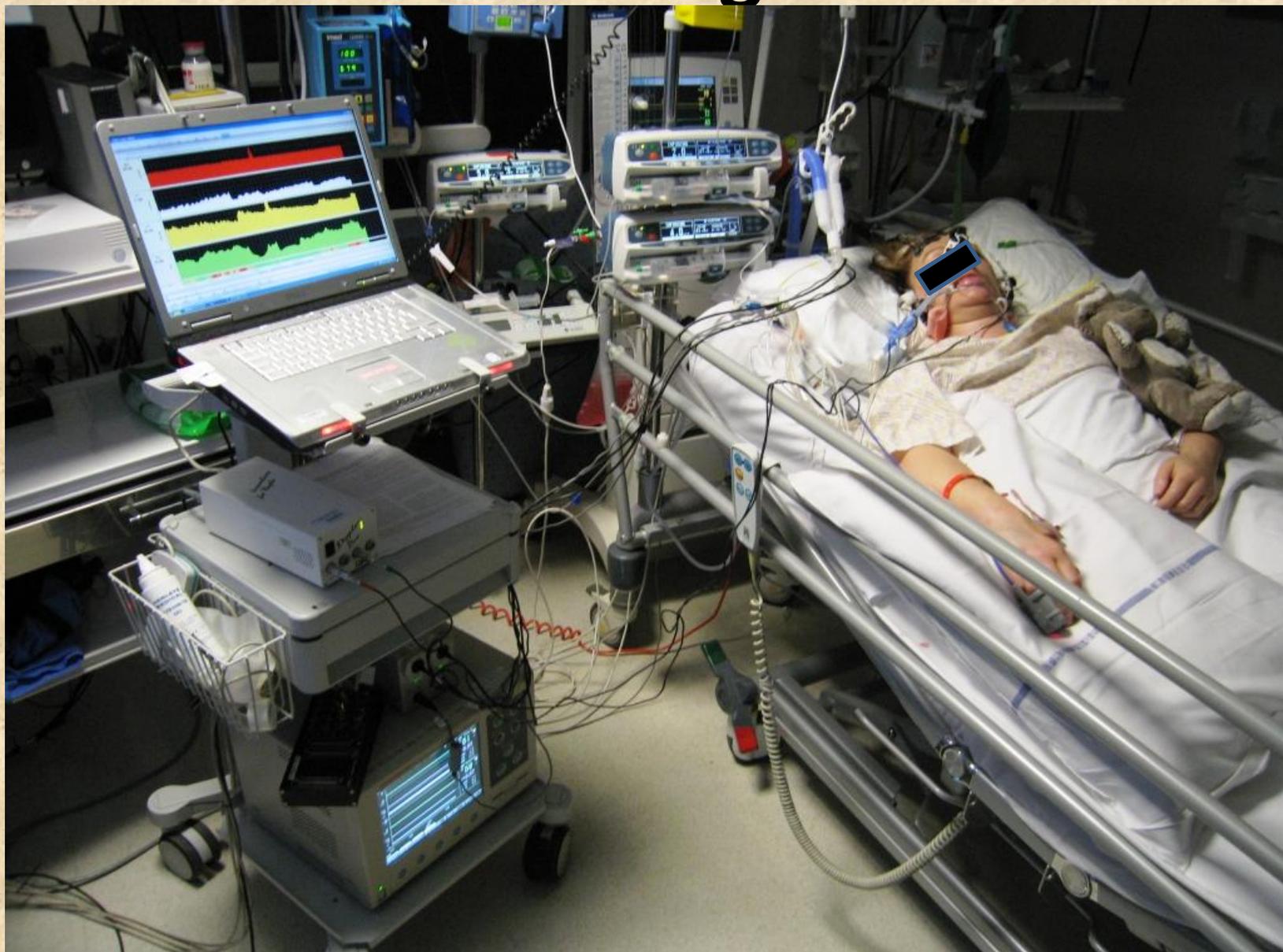
Thanks to Dr.P.Smielwski

# Transient Hyperaemic Response Test Test repeated at different CO<sub>2</sub> levels

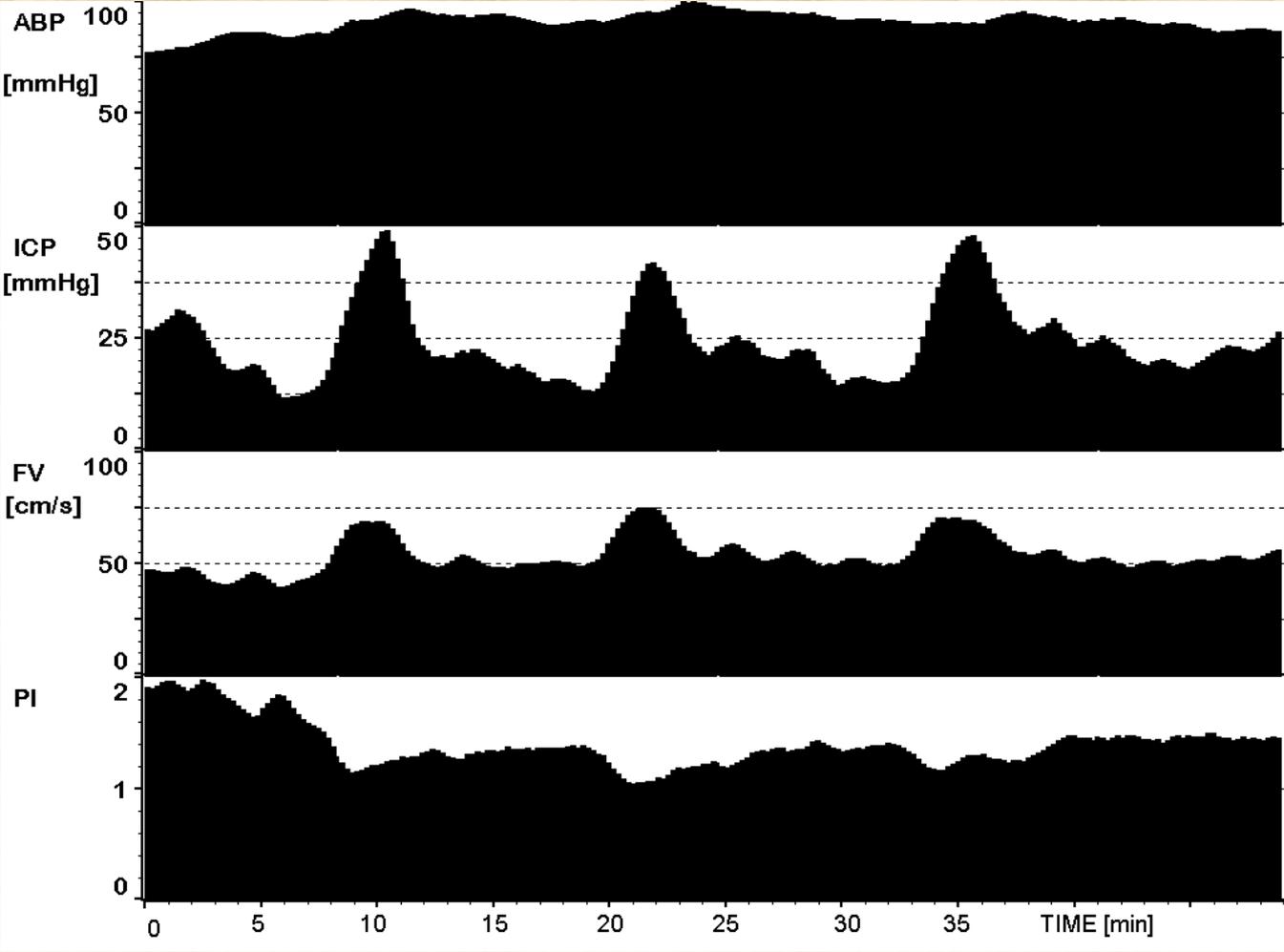


Thanks to Dr.P.Smielwski

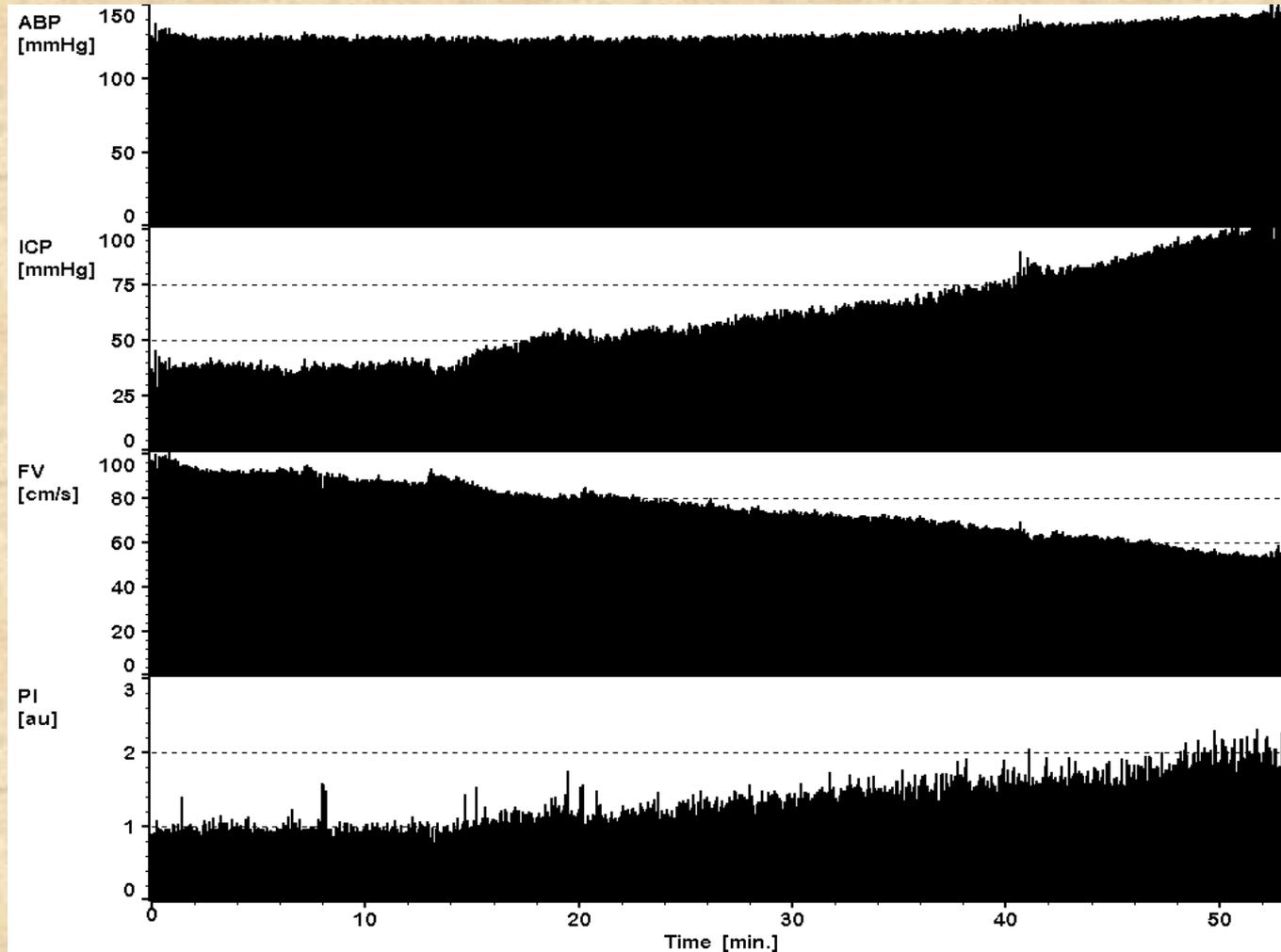
# Brain monitoring on NCCU



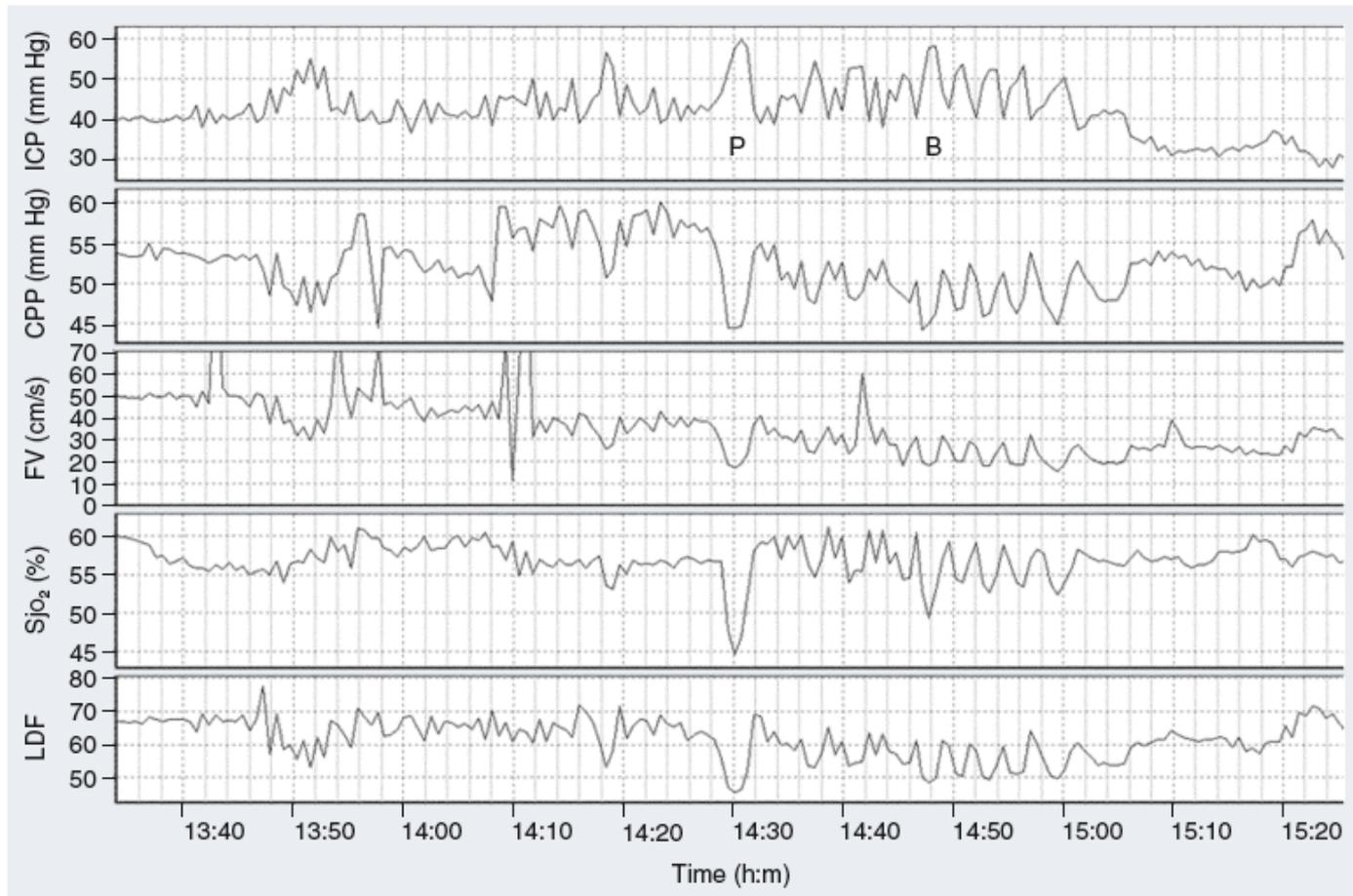
# Continuous monitoring of CBF: 'Hyperaemic' waves of ICP



# Refractory intracranial hypertension:

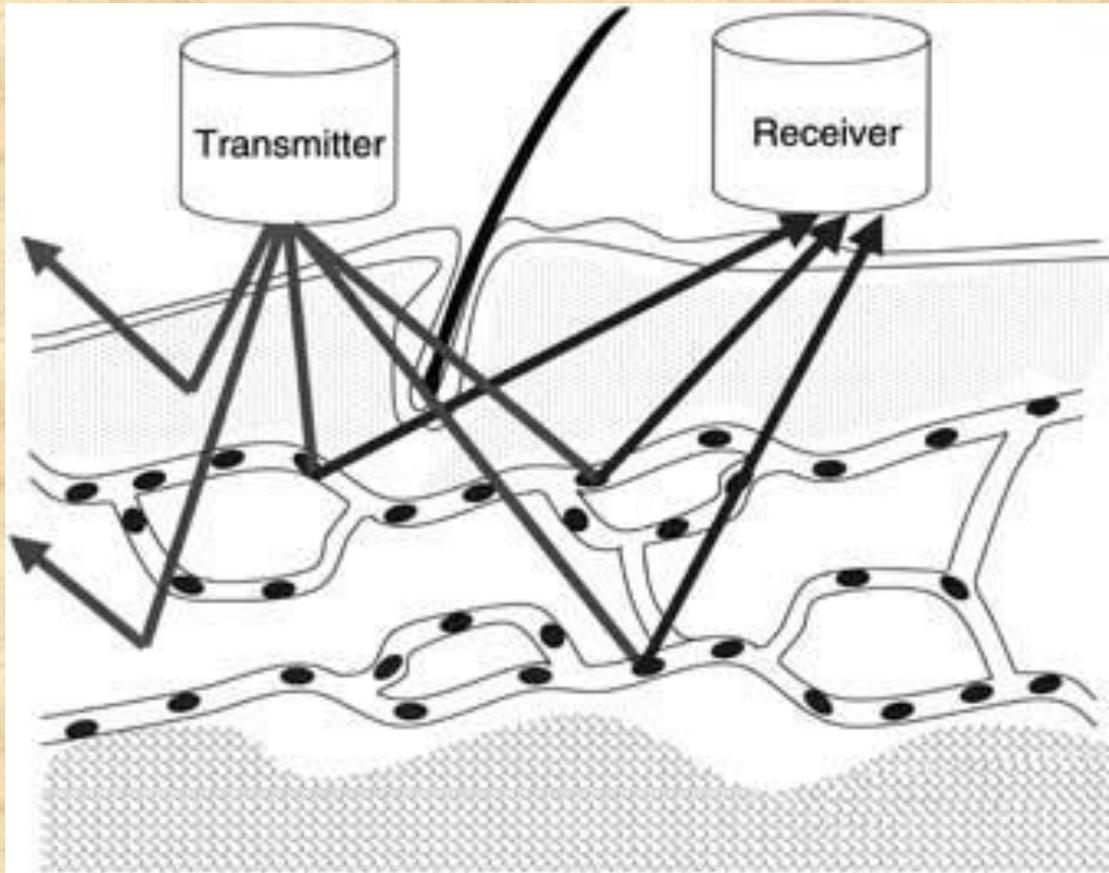


# Multimodal CBF monitoring



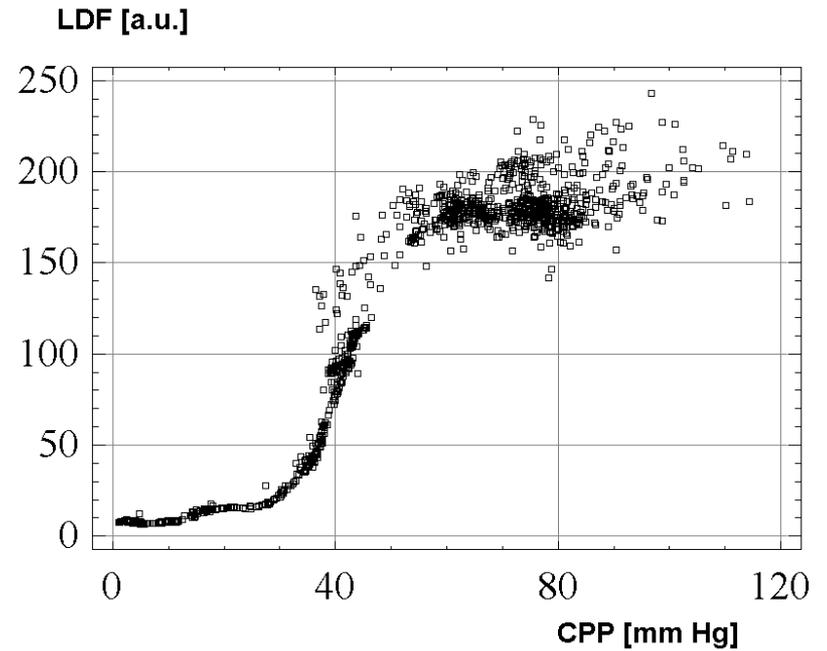
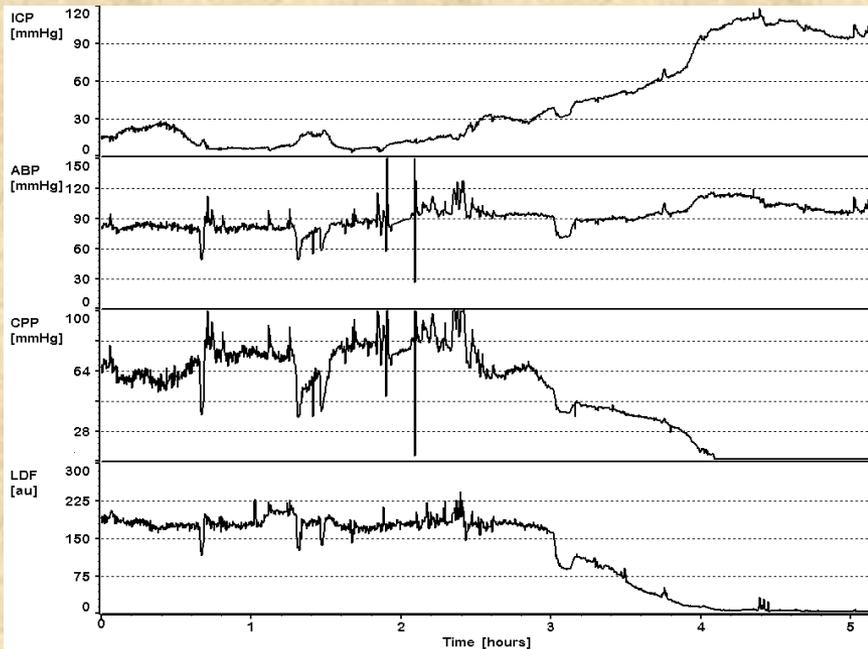
**Figure 8-8** Recording of events characterized by intracranial hypertension in a head-injured patient receiving intensive care. Using multimodality monitoring makes it possible to identify the cause of this increase. Increase in intracranial pressure (ICP) (plateau wave [P]) is secondary to a fall in cerebral perfusion pressure (CPP), as the blood velocity (FV), the jugular bulb oxygen saturation values (Sj<sub>o</sub><sub>2</sub>) and cortical blood flow (LDF, in arbitrary units) also fall, indicating hypoperfusion. Repetitive vasogenic waves of ICP (B waves [B]) are secondary to fluctuations of cerebral blood flow as Sj<sub>o</sub><sub>2</sub>, and FV, and LDF increase and decrease in phase with ICP.

# Laser Doppler Flowmetry



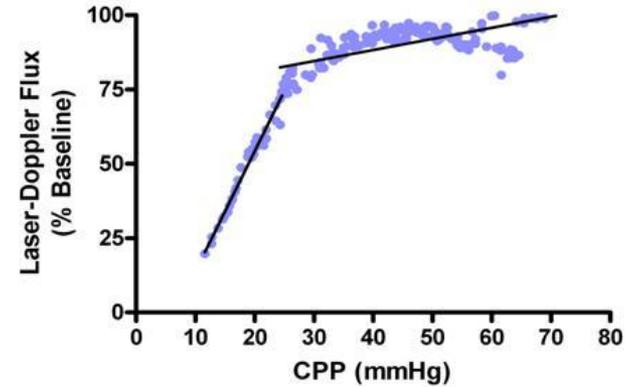
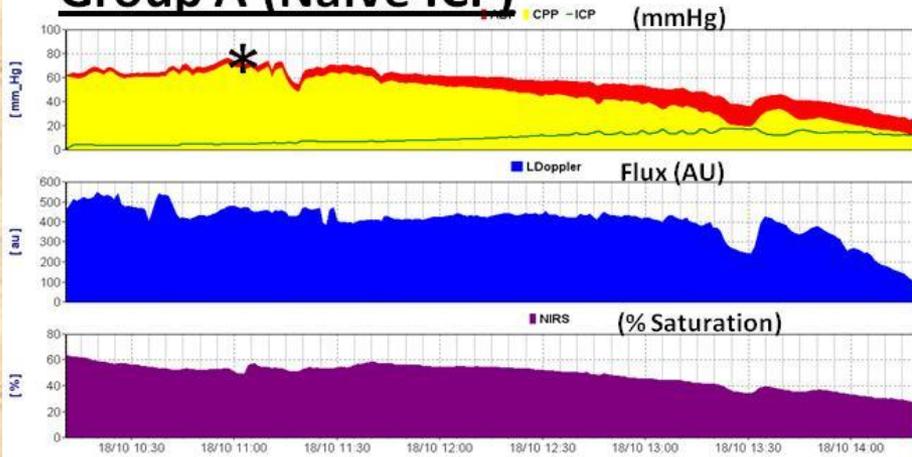
**Figure 1** Basic operating principles of laser Doppler flowmetry. A laser beam is directed to an area of tissue. Upon contact with red blood cells in the target tissue, light waves are reflected and scattered, resulting in broadening of the light wave frequency, which is detected and received by a photodetector.

# Clinical monitoring of rCBF using LDF

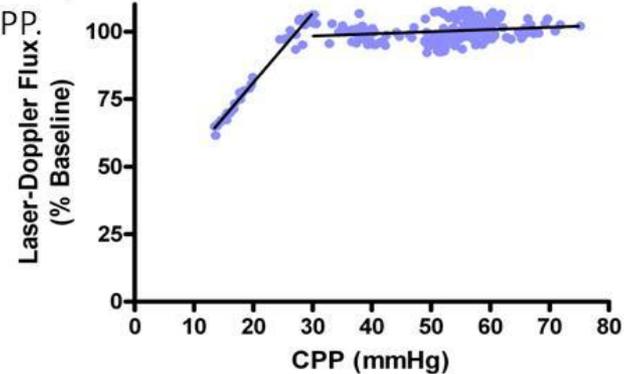
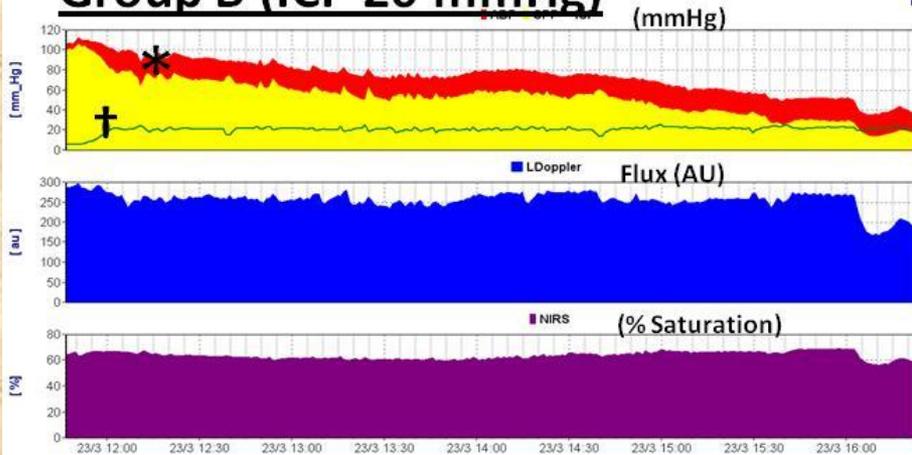


# Experimental monitoring

## Group A (Naïve ICP)



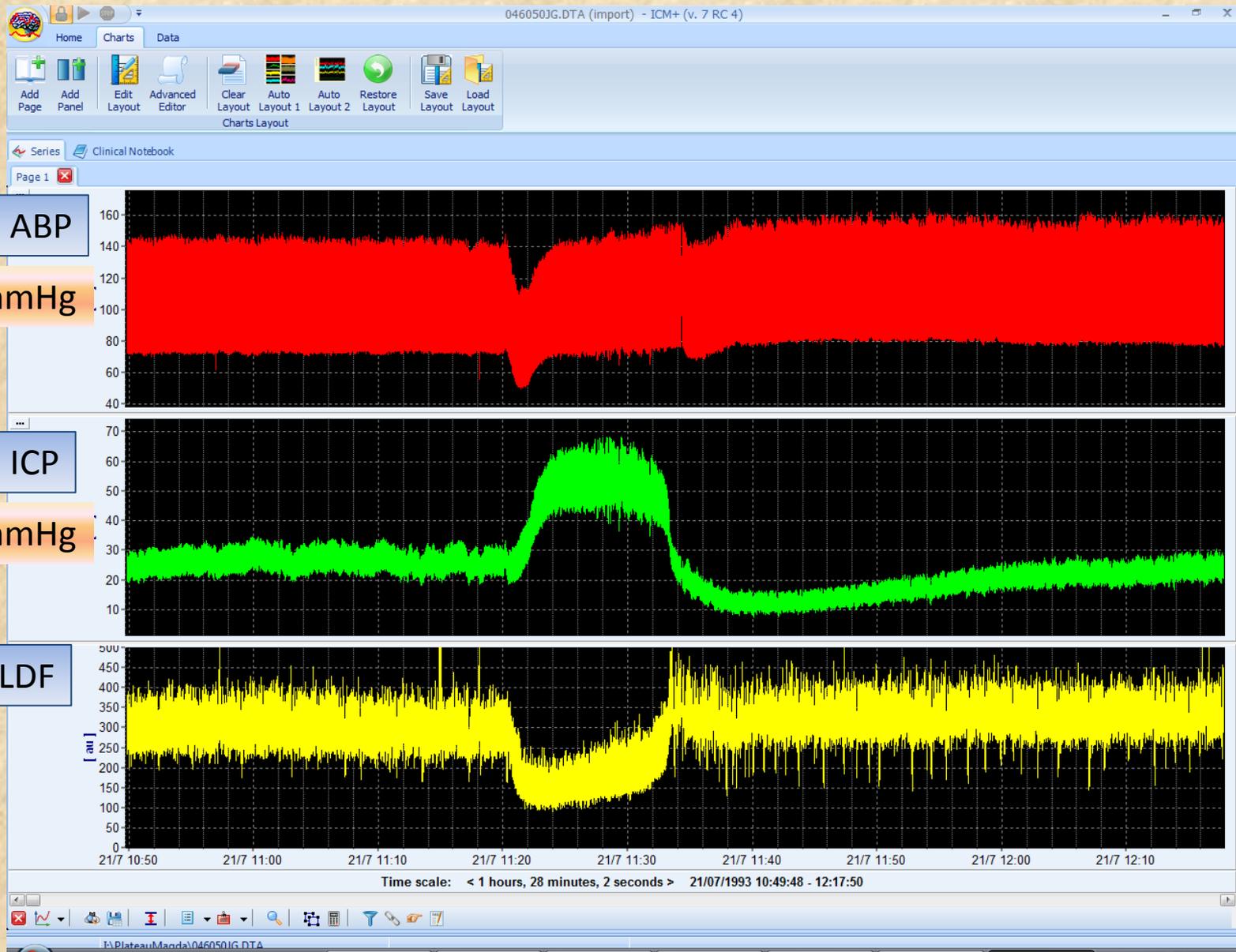
## Group B (ICP 20 mmHg)



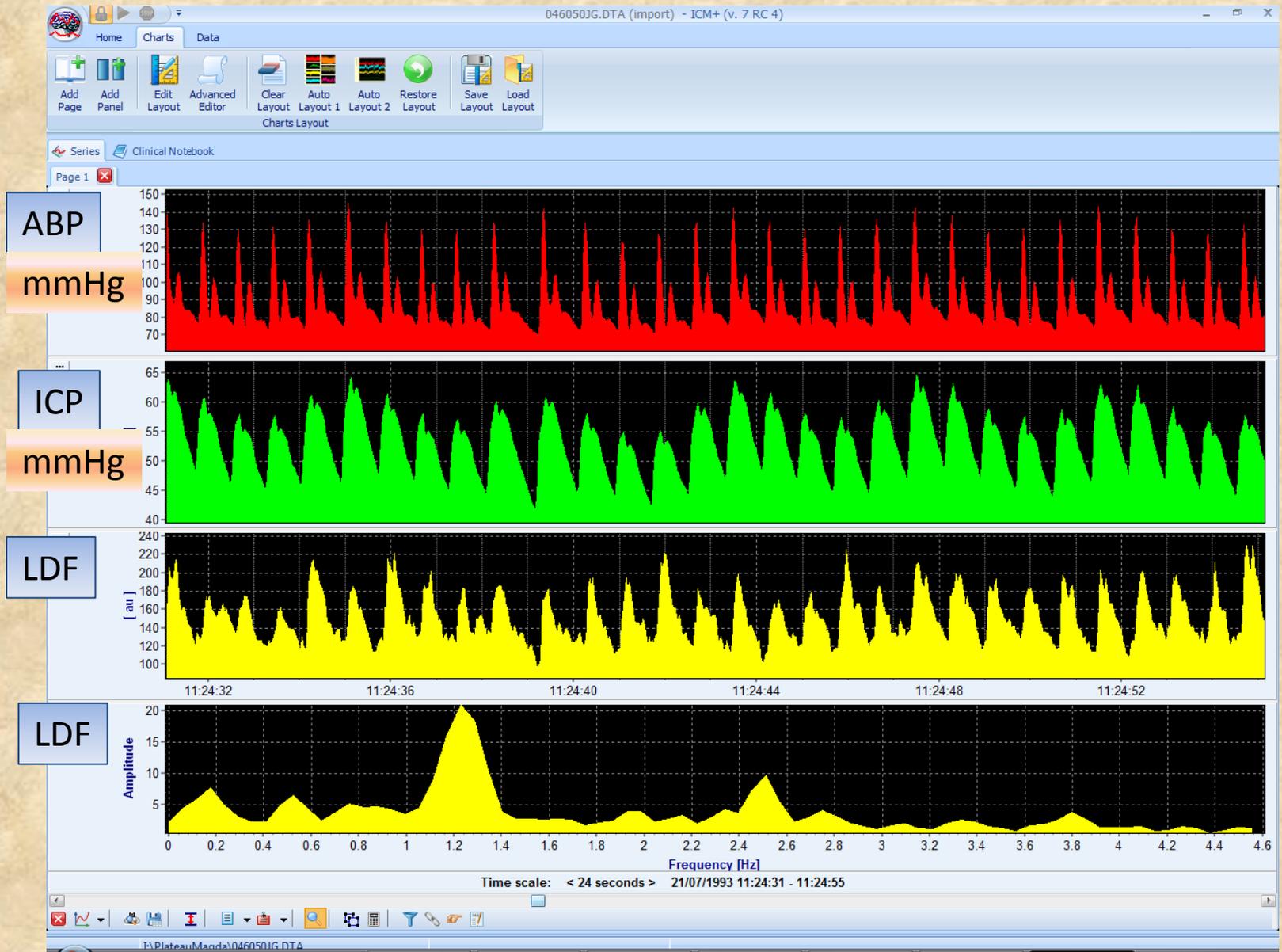
The LLA is the intersection of the two best-fit lines with the lowest residual error squared taken from plots of CBF against CPP.

Thanks to Dr. K.Brady

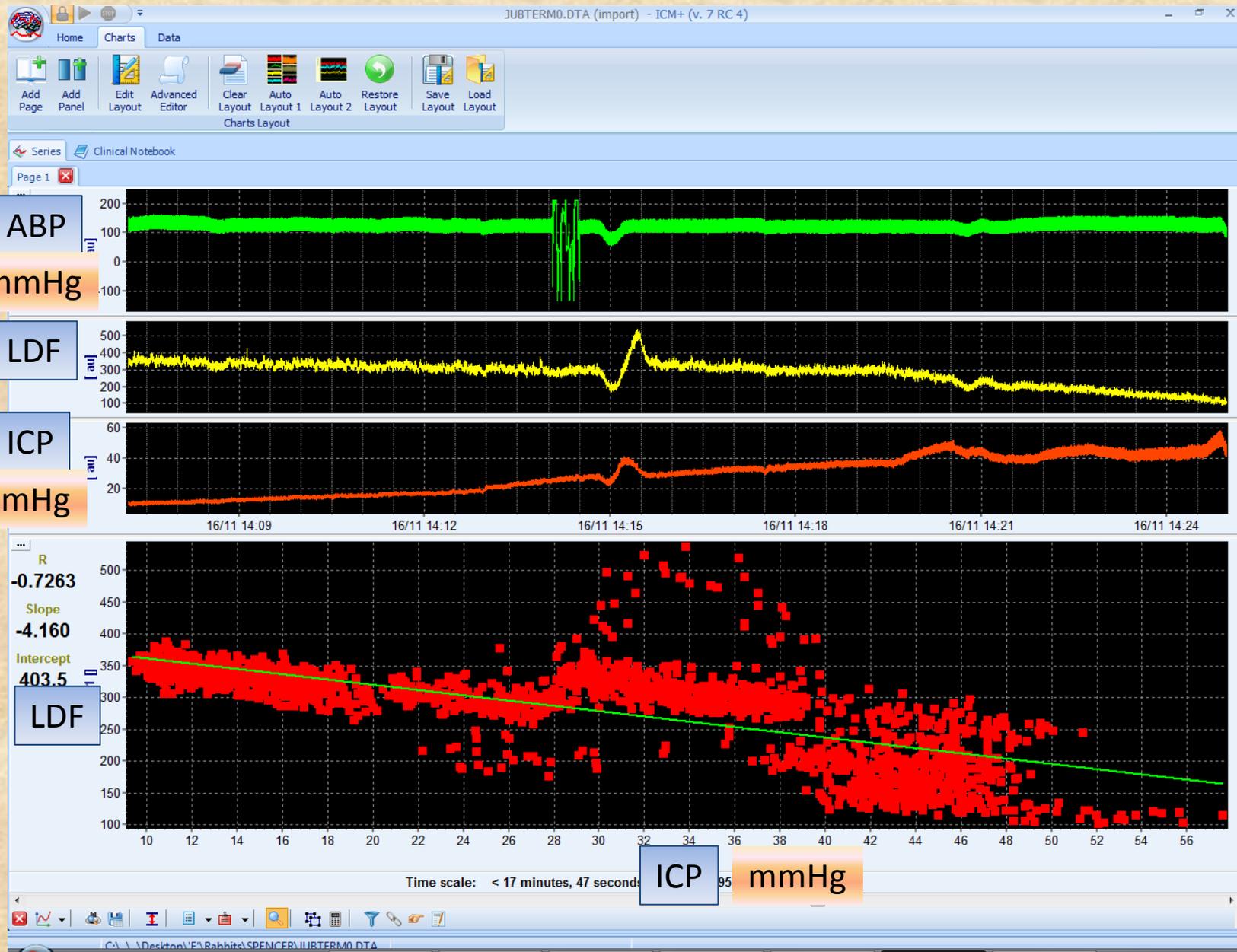
# LDF flux during plateau elevation of ICP

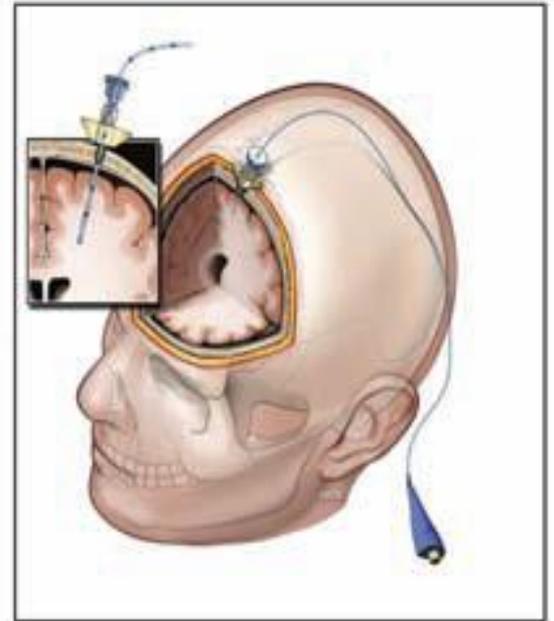
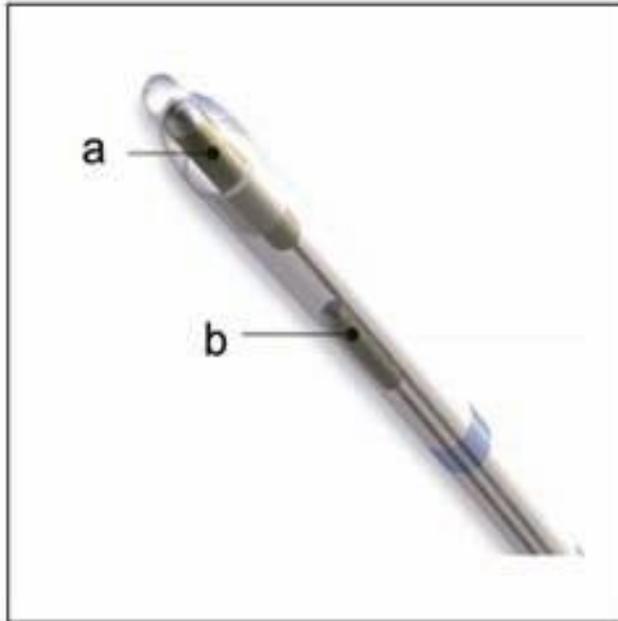
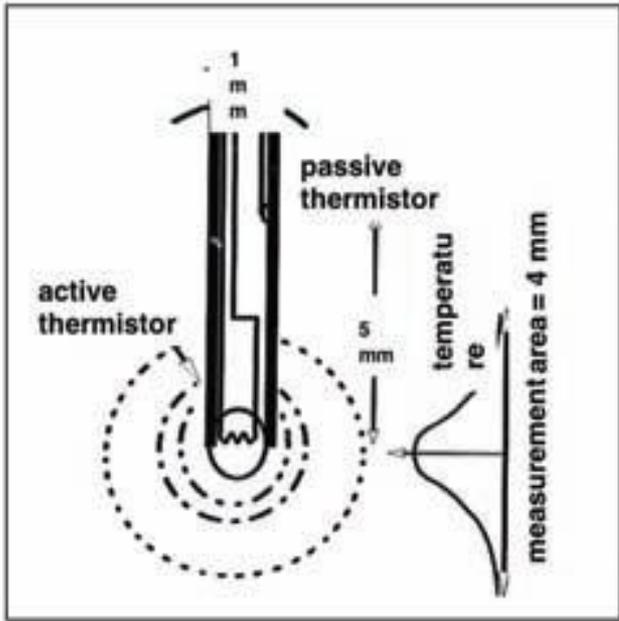


# 'Pulse wave' of LDF flux



# LDF during refractory elevation of ICP





- Měření v absolutních jednotkách (ml/100 g/min)
- Monitorování u lůžka pacienta
- Neopletčný očečet údajů v reálném čase

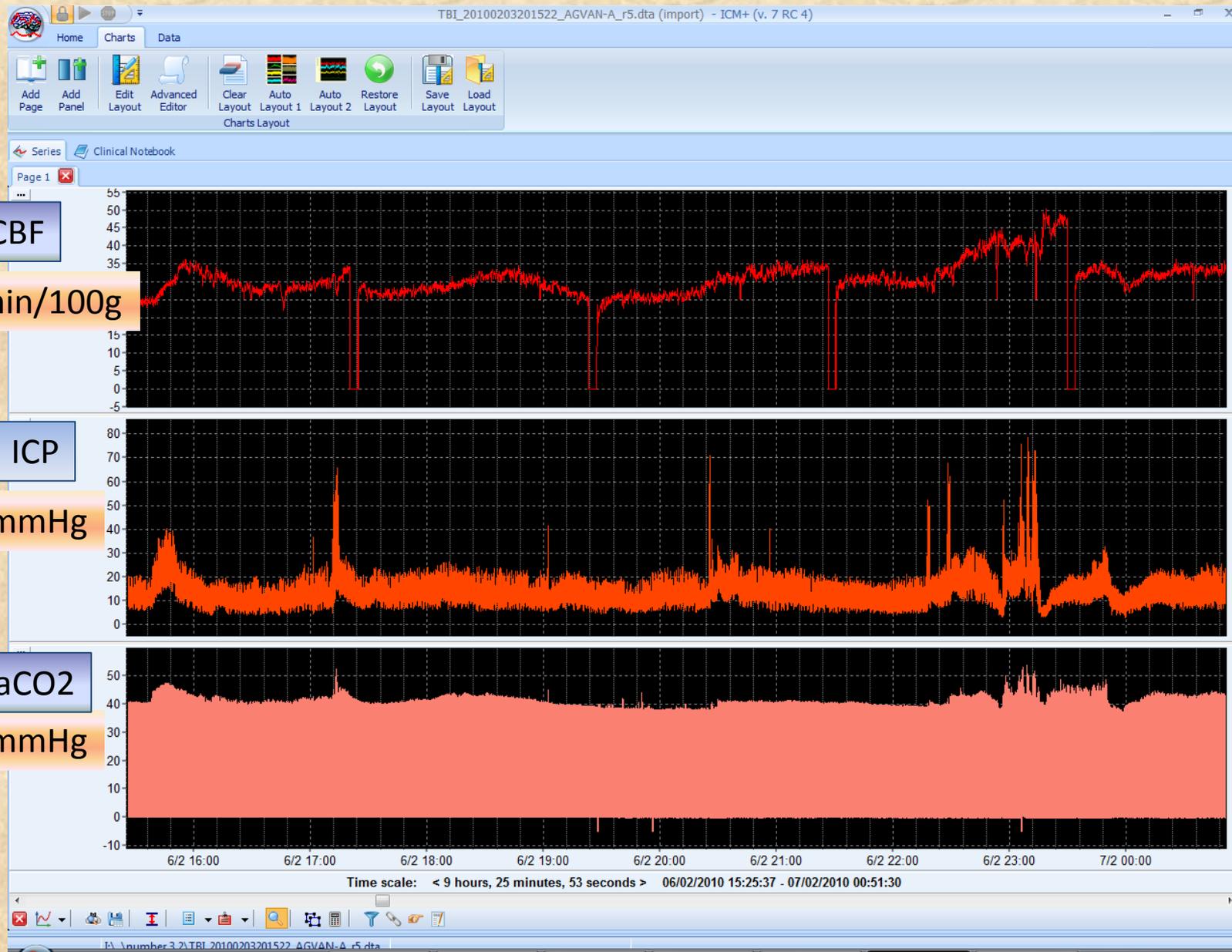
Zatímco ostatní systémy zaznamenávají relativní změny, Hemedex poskytuje absolutní měření průtoků. Změny jsou porovnány s kvalitativně předdefinovanými.

Když vyšetření probíhá, lze měření provádět i při změně polohy pacienta. Měření lze provádět i u pacientů s poruchami srdečního rytmu.

Měření se provádí kontinuálně a v reálném čase. Vytváří se tak nepřerušovaný záznam průtoků. Údaje lze rychle a snadno uložit a přenést do počítače.

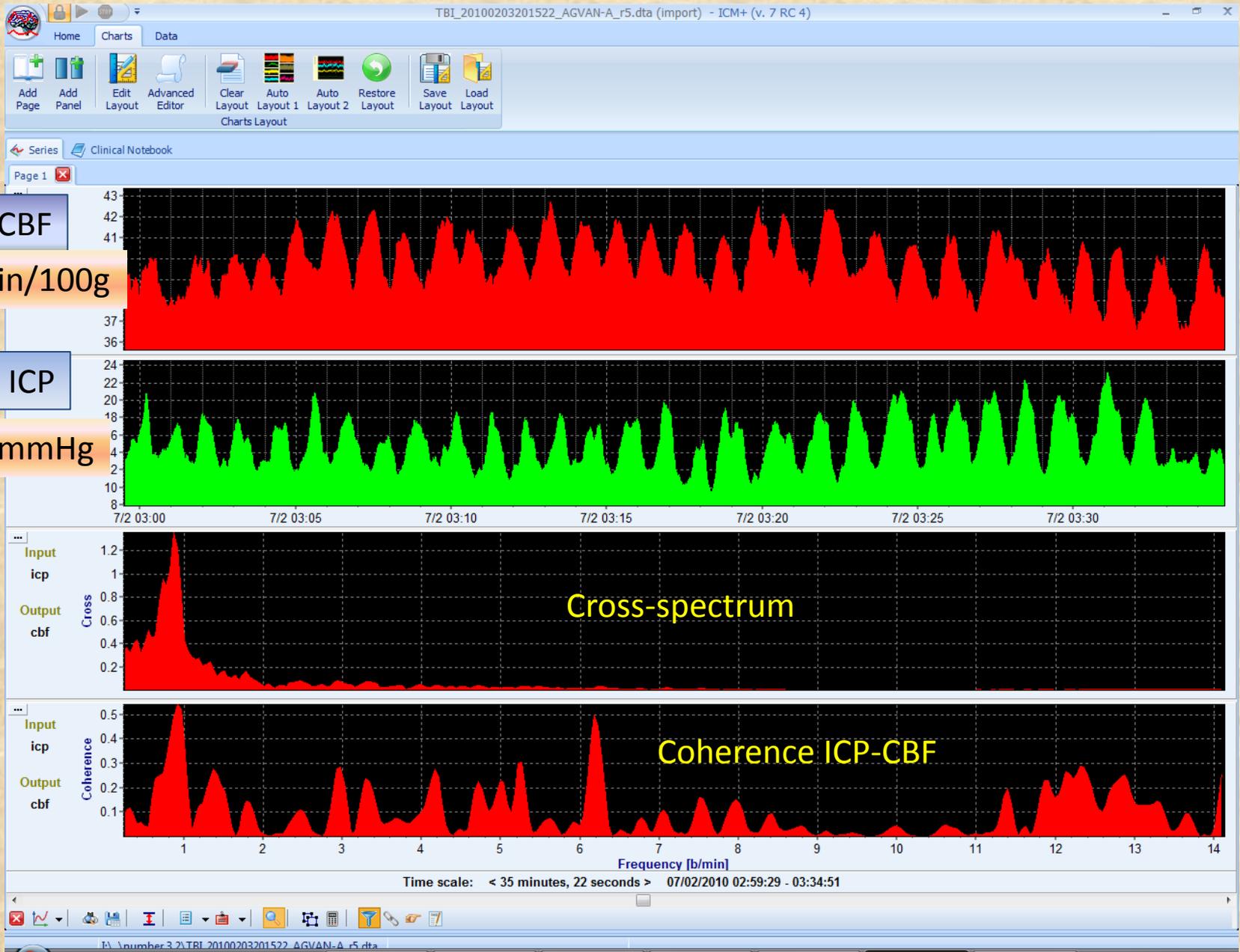
## Hemedex- rCBF measurement using thermal dilution method

# Changes in Hemedex CBF related to changes in EtCO2

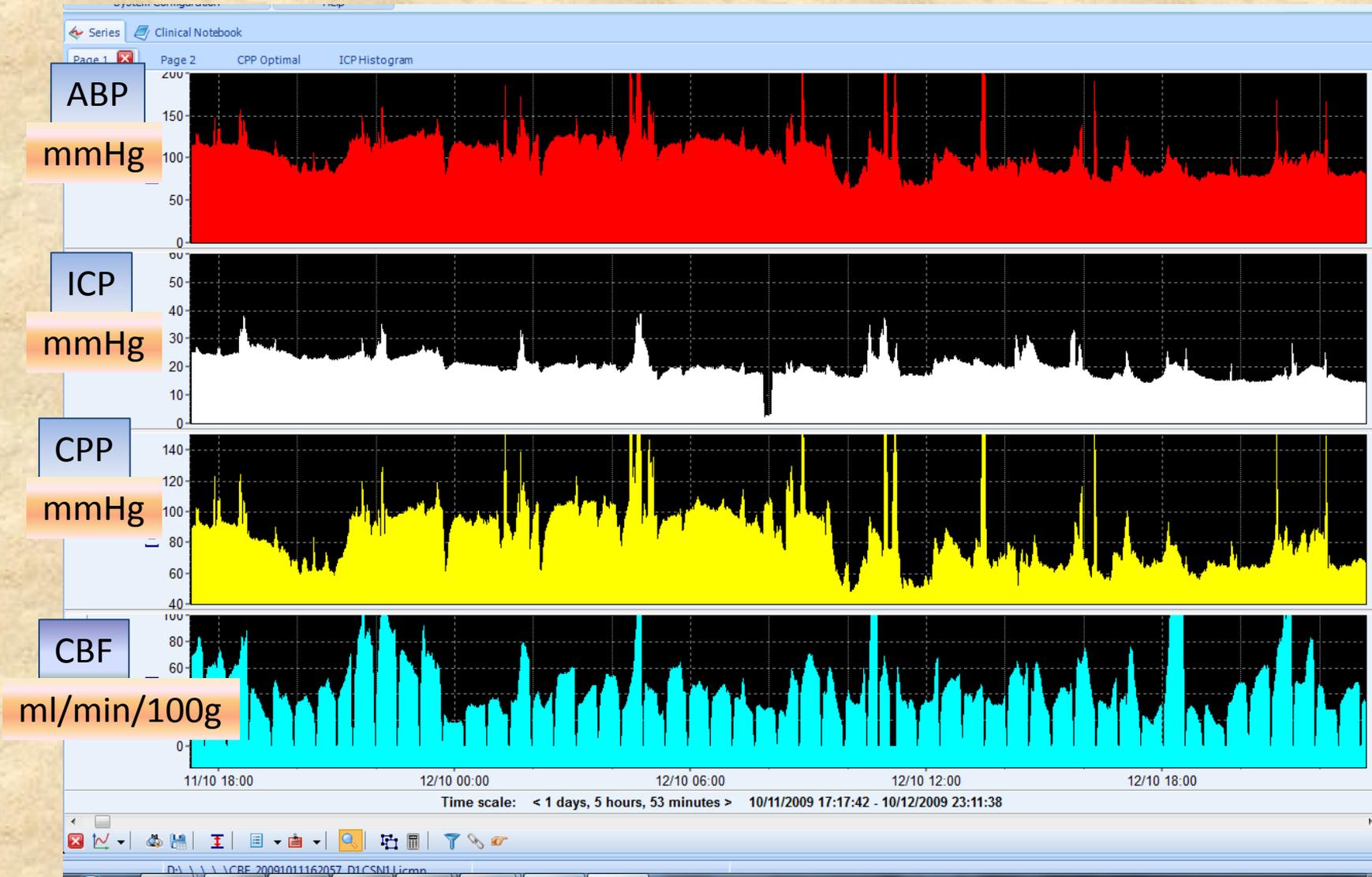


Thanks to Dr A.Oshorov

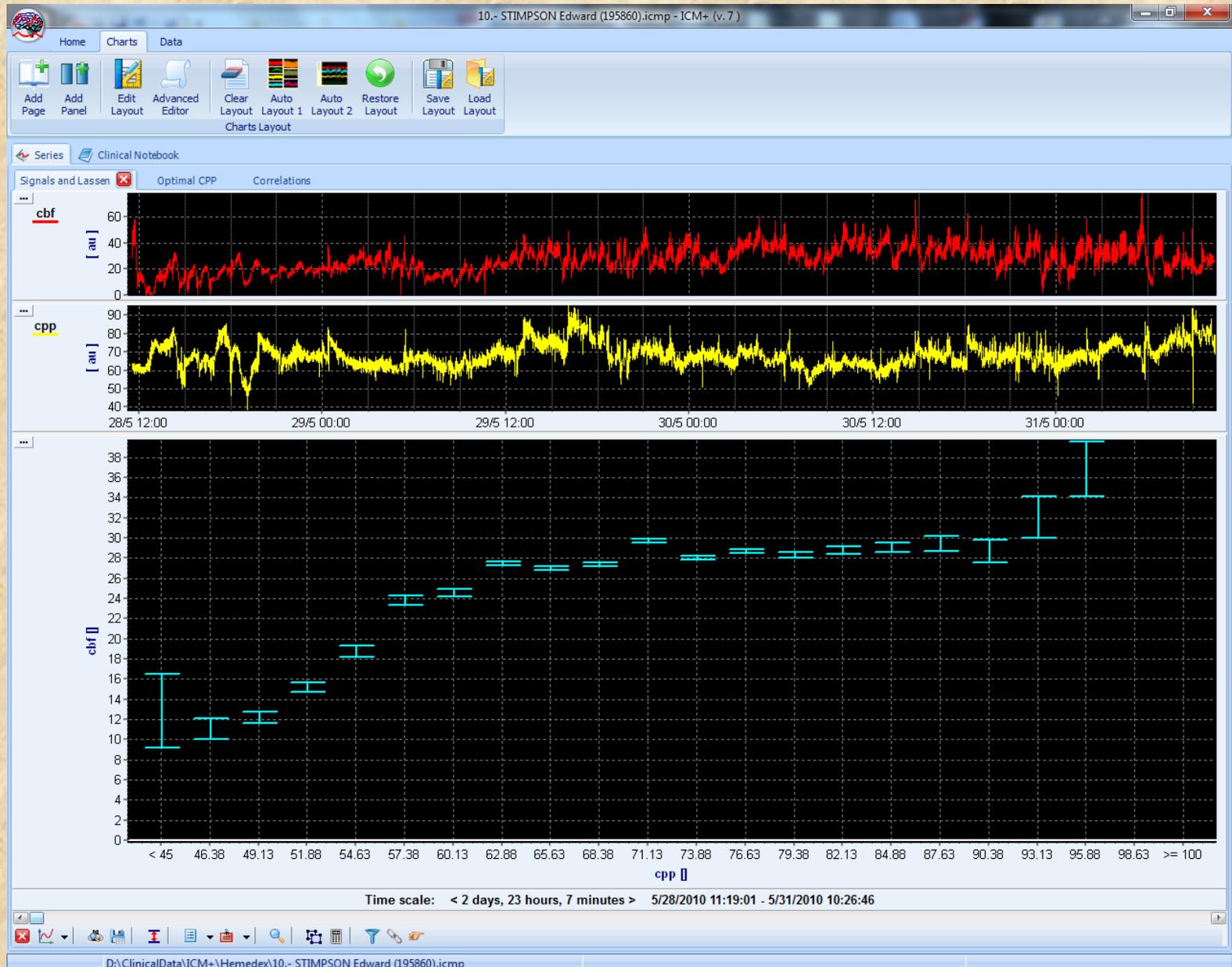
# Slow waves in Hemedex CBF and ICP



# Head injury- CBF fluctuates independently on CPP

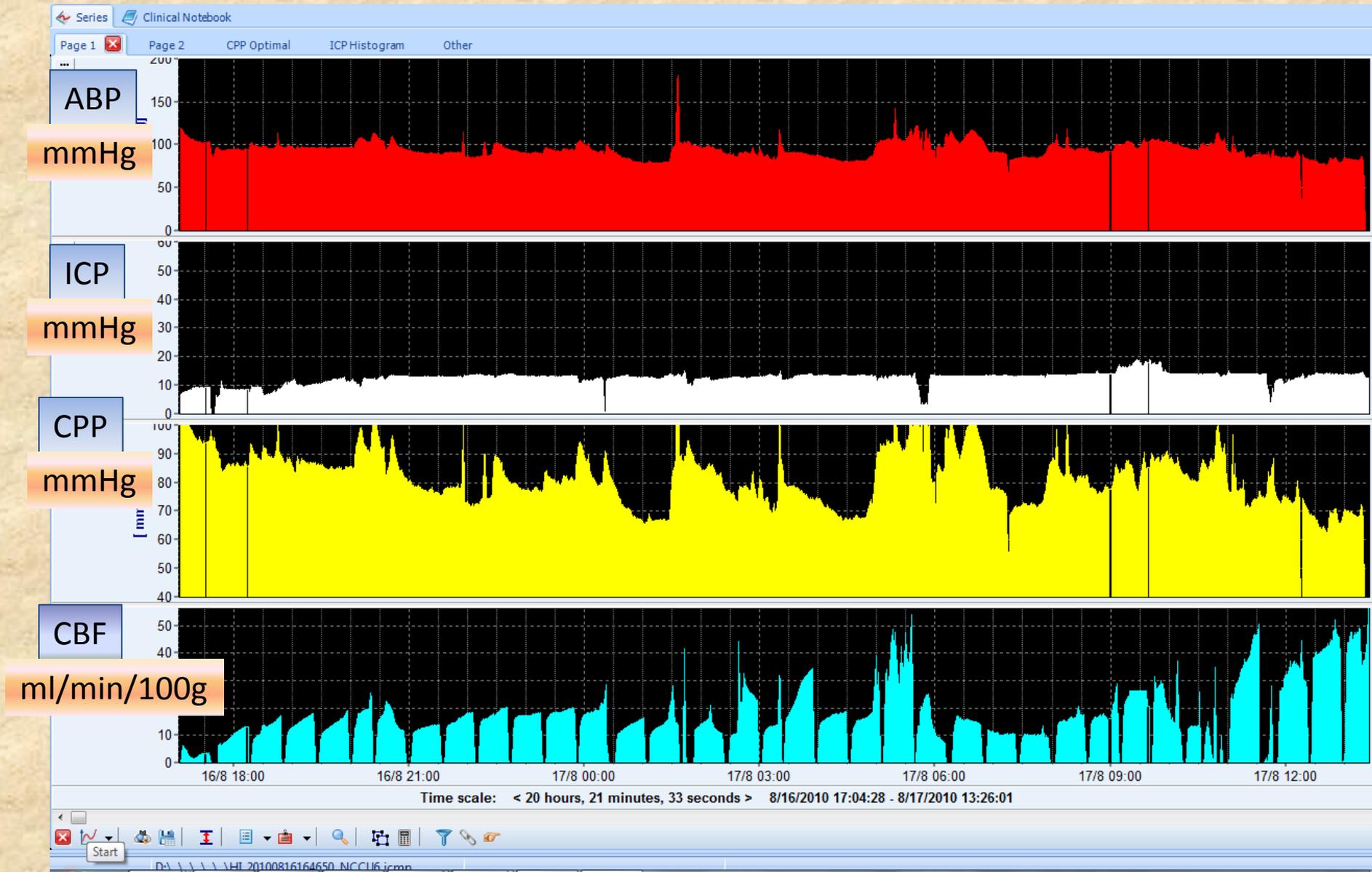


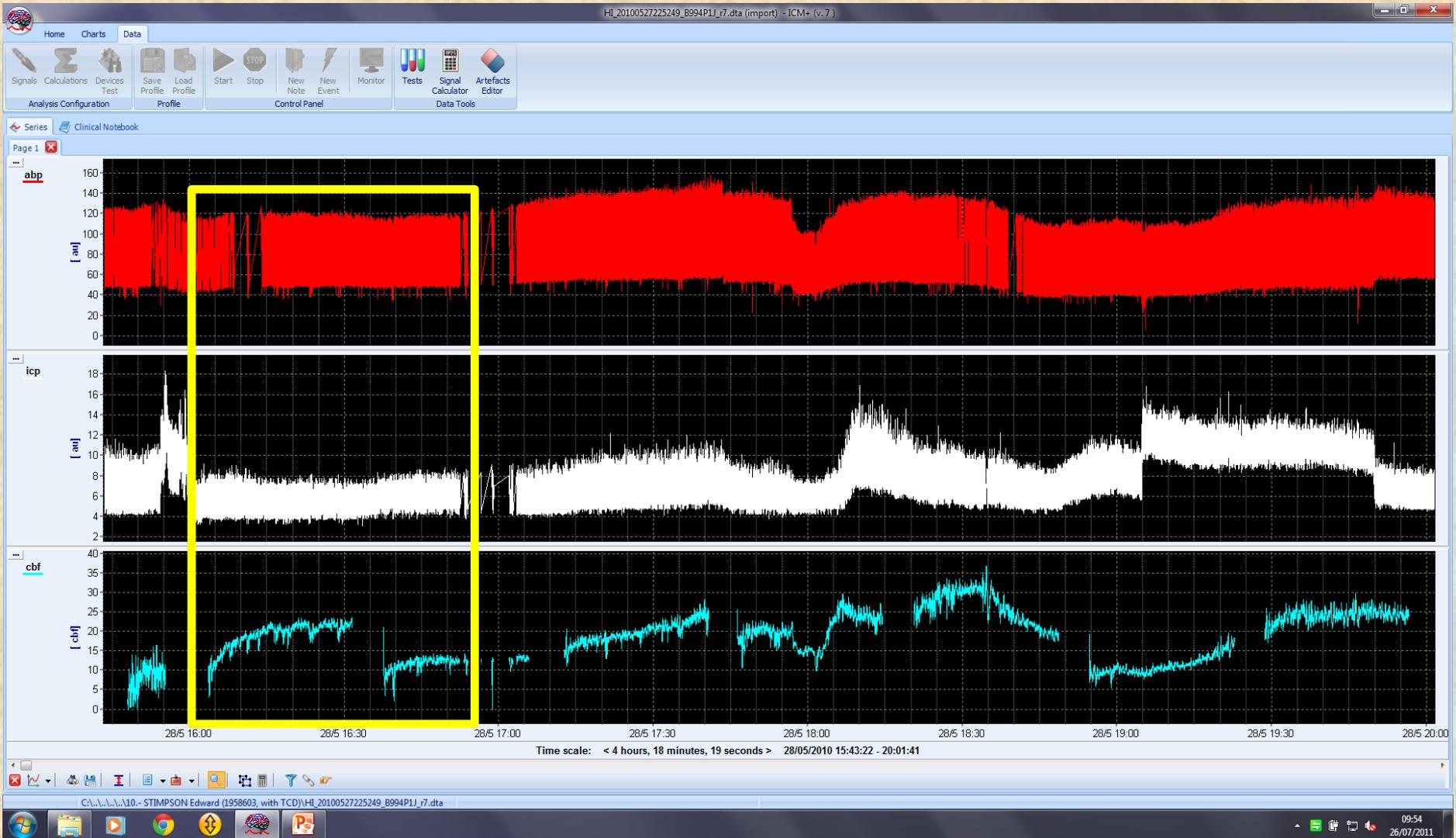
# But not always: example of homogenous Lassen's curve; 3 days monitoring , TBI



Thanks to Dr. N. De Riva Solla

# Calibration gaps- main source of variation in measured CBF





Typical...

Thanks to Dr. N. Der Riva Solla

# Message to take home

TCD- non-invasive, indirect and difficult in continuous monitoring

TCD- information included in mean velocity and waveform

TCD- very good dynamical response

LDF- invasive, indirect

LDF- rarely used in clinical practice

LDF- biological zero

Hemedex- invasive, direct

Hemedex- lot of fluctuations which seem to be artificial

