

A human corneal endothelium equivalent constructed with acellular porcine corneal matrix

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Background & objectives: Artificial corneal endothelium equivalents can not only be used as *in vitro* model for biomedical research including toxicological screening of drugs and investigation of pathological corneal endothelium conditions, but also as potential sources of grafts for corneal keratoplasty. This study was aimed to demonstrate the feasibility of constructing human corneal endothelium equivalents using human corneal endothelial cells and acellular porcine corneal matrix.

Methods: Porcine corneas were decellularized with sodium dodecyl sulphate (SDS) solution. Human corneal endothelial cells B4G12 were cultured with leaching liquid extracted from the acellular porcine corneal matrix, and then cell proliferative ability was evaluated by MTT assay. B4G12 cells were transplanted to a rat corneal endothelial deficiency model to analyze their *in vivo* bio-safety and pump function, and then seeded and cultured on acellular porcine corneal matrix for two wk. Corneal endothelium equivalents were analyzed using HE staining, trypan blue and alizarin red S co-staining, immunofluorescence and corneal swelling assay.

Results: The leaching liquid from acellular porcine corneal matrix had little influence on the proliferation ability of B4G12 cells. Animal transplantation of B4G12 cells showed that these cells had similar function to the native cells without causing a detectable immunological reaction and neoplasm *in vivo*. These formed a monolayer covering the surface of the acellular porcine corneal matrix. Trypan blue and alizarin red S co-staining showed that B4G12 cells were alive after two wk in organ culture and cell boundaries were clearly delineated. Proper localizations of ZO-1 and Na⁺/K⁺ ATPase were detected by immunofluorescence assay. Functional experiments were conducted to show that the Na⁺/K⁺ ATPase inhibitor ouabain could block the ionic-pumping function of this protein, leading to persistent swelling of 51.7 per cent as compared to the control.

Interpretation & conclusions: Our findings showed that B4G12 cells served as a good model for native corneal endothelial cells *in vivo*. Corneal endothelium equivalents had properties similar to those of native corneal endothelium and could serve as a good model for *in vitro* study of human corneal endothelium.

Key words Biomaterial - corneal endothelium - decellularized carrier - organ culture

Of the three major cell layers of course, the innermost monolayer of specialized endothelial cells maintains corneal transparency by its barrier function and pump-leak mechanism. Endothelial cells maintain stroma dehydration at 78% by transporting ions and fluid across the cell membranes. Since this is an active and energy-consuming process, it is described as “pump function”. And the protein Na^+/K^+ ATPase mainly involved in this process is called the “pump protein”. The number of adult human corneal endothelial cells (CECs) decreases with age due to the limited proliferative capacity of these cells. CECs loss and dysfunction, resulting from inflammation, accidental damage during cataract surgery or as an inherited condition, can lead to progressive corneal swelling and formation of epithelial bullae, causing severe pain and even blindness.

Numerous *in vitro* and *in vivo* studies concerning corneal endothelium protection and proliferation have recently been conducted¹⁻³. However, the improvement of strategies to overcome the corneal epithelial barrier and blood-aqueous humor barrier for targeted drug delivery to the corneal endothelium remains a major challenge. Corneal endothelium equivalents now offer a good opportunity for toxicological screening of drugs and investigation of pathological corneal endothelium conditions. Also, corneal endothelium equivalents could be substitutes for experiment animals for *in vivo* studies. These could also be a potential source of grafts for corneal endothelial keratoplasty and might solve the problem of supply shortage of donor corneas⁴.

The construction of corneal endothelium equivalents requires recruitment of active CECs and a scaffold. Bioengineered corneal endothelium still faces many difficulties, including the lack of source of CECs and the failure of scaffolds to meet clinical demands such as biocompatibility, transparency, and mechanical strength.

Limited accessibility and proliferative ability of primary human CECs make *in vitro* studies of these cells difficult. Human corneal endothelial cell line could be steadily passaged *in vitro*⁵. B4G12 cells, one of the two clonal subpopulations, showed good similarities to their natural counterparts, and thus could be a promising substitute candidate for human CEC⁵. But application of B4G12 cells in corneal endothelium equivalent construction still requires further analysis regarding bio-safety and pump function *in vivo*.

At present all the scaffolds can be classified into natural and synthetic materials. Natural membranes such

as amniotic membranes^{6,7} or Descemet's membranes^{8,9} are too thin to handle, while synthetic polymers may have poor graft-host integration and biocompatibility¹⁰. Due to its unique extracellular matrix organization, the cornea itself came to be an ideal candidate. The porcine cornea appears to be particularly attractive because of its anatomic similarity to the human cornea¹¹. Different methods have been tried to acquire decellularized porcine corneal scaffold over many years. Although methods of tissue decellularisation have been used in a variety of applications, such as adipose, skeleton muscle, urinary bladder and cardiovascular tissue engineering and regeneration¹²⁻¹⁶, but there are not many reports of their use to produce an acellular corneal scaffold. Fu *et al*¹⁷ acquired an acellular porcine corneal matrix scaffold using Triton X-100, but they did not achieve complete cell clearance by this protocol. Choi *et al*¹⁸ created decellularized human corneal stroma scaffolds using Triton X-100, which was cell-free and similar to natural cornea in structure, mechanical toughness and optical characters. But the bioengineered corneal endothelium still has to rely on human donor corneas, which are not easily available. An acellular porcine corneal matrix (APCM) was recently created using sodium dodecyl sulphate (SDS) according to the protocol developed in our laboratory¹⁹⁻²¹. The mechanical, ultrastructural and biological properties of this scaffold were studied in detail, and APCM proved to be a suitable scaffold for corneal equivalent construction¹⁹⁻²⁴.

In this study, the bio-safety and pump function of BG12 cells were tested *in vivo* through a rat corneal endothelial deficiency model. B4G12 and APCM were used to show the possibility of constructing a corneal endothelium equivalent under serum-free condition for *in vitro* study.

Material & Methods

This study was conducted in the Key Laboratory of Cardiovascular Remodeling and Function Research, Qilu Hospital, Shandong University.

Adult porcine eyes were obtained from a local slaughterhouse (Jinan Welcome Food Co., Ltd, Jinan, PR China) within 3 h post-mortem, and subjected to decellularization procedure within 1 h of acquisition.

The chemicals used were SDS, human recombinant bFGF, chondroitin-6 sulphate, laminin, trypsin-EDTA, alizarin red S, goat serum, and DAPI (Sigma, USA), human endothelial SFM, proteinase inhibitor and rabbit anti-human ZO-1 Mab (Invitrogen, USA), carboxyfluorescein diacetate, succinimidyl ester

(Beyotime, China), mouse anti-human Na⁺/K⁺ ATPase (Santa Cruz, USA), optimal cutting temperature compound, goat anti-rabbit IgG conjugated with FITC and goat anti-mouse IgG conjugated with FITC (Beijing Zhongshan, China). Microplate reader was purchased from InTec Reader (USA), slit lamp microscope and inverted light microscope from Zeiss (Germany), and fluorescence microscope was purchased from Olympus (Japan). In vitro specular microscope was purchased from Alcon (USA).

Animals: Twenty Sprague Dawley (SD) rats (Center for New Drugs Evaluation of Shandong University, Jinan, PR China) weighing 250-350 g were used for animal transplantation. The research protocol was approved by the ethical committee for animal experiments of Qilu hospital, Shandong University, and all animals were treated according to the national and international rules of animal welfare, including the ARVO Statement for the Use of Animals in Ophthalmic and Vision Research.

Decellularization of porcine corneas: Fresh porcine eyes were washed with 1 per cent penicillin-streptomycin in phosphate-buffered saline (PBS, pH 7.2-7.4) and the corneas were dissected under sterile condition. Briefly, a single cornea was cut into a 10 mm diameter button with a trephine. Corneal buttons were then immersed in 0.5 per cent (wt./vol.) SDS solution with a solvent/tissue mass ratio of 20:1 (vol. /wt.). They were placed on an orbital shaker for 24 h at 4 °C and rinsed 8 times in sterile PBS for 16 h. Finally, APCMs were washed 3 times in sterile PBS supplemented with 200 U/ml penicillin and 200 U/ml streptomycin for 3 h, freeze-dried at -20 °C for 12 h, air-dried at room temperature for 3 h in a biological safety cabinet, and stored at -20 °C before use. All steps were conducted under sterile conditions.

Cell culture: The human corneal endothelial cell line was first created in 2000, and detailed information about two cell subpopulations was also investigated²². B4G12 cells (generously provided by Monika Valtink as a gift) were cultured according to the previous protocol^{22,23}. Briefly, B4G12 cells were cultured in human endothelial-SFM supplemented with 10 ng/ml human recombinant bFGF in T25 culture flasks coated with 1 mg chondroitin-6 sulphate and 10 µg laminin. Cells were passaged using 0.05 per cent trypsin-0.02 per cent EDTA at 37 °C for 1 min. Enzyme activity was quenched by proteinase inhibitor.

Cytotoxicity of extractable materials: Each scaffold was extracted using 5 ml B4G12 culture medium at 37 °C

for 48 h. A cell suspension of B4G12 was added to 96-well plates at a density of 8×10^3 /well and cultured with the leaching liquid (the experimental group, n=6) or the normal medium (control group, n=6) respectively. Cells were cultured at 37 °C and 5% CO₂. After 1, 3, 5, and 7 days, the proliferation activity of the cells was quantitatively determined by MTT assay¹⁹. The optical density (OD) of absorbance at 490nm was measured by a microplate reader. Differences in the OD value between experimental and control groups were statistically analyzed using one-way ANOVA.

Anterior chamber injection of B4G12 cells in the rat model of corneal endothelium deficiency: The SD rat model of corneal endothelium deficiency was used for B4G12 cell transplantation to determine their bio-safety and pump function *in vivo*. The procedure was conducted according to the previous method^{24, 25}. Briefly, SD rats were anaesthetized with intraperitoneal injection of 10 per cent chloral hydrate (0.3 ml/100 g). The cornea of the right eye was treated for 15 sec by immediately placing a brass dowel that had been cooled in liquid nitrogen on the surface. This procedure was repeated twice, each time allowing the eyeball to thaw by saline irrigation prior to refreezing. The anterior chamber was carefully washed three times with saline through a 0.5 mm width paracentesis. B4G12 cells were labelled with a kind of fluorescent dye called carboxyfluorescein diacetate, succinimidyl ester (CFDA SE). Then 8.5×10^4 cells (for a rat cornea of 6mm in diameter corresponding to a seeding density 3000 cells/mm², n=8) were injected into the anterior chamber of each right eye, and cryoinjury only served as the control group (n=8). Both test and control groups of rats were kept in the eye-down position for 24 h under deep anaesthesia. Each surgical eye was checked and photographed with a slit lamp microscope three times a week for one month. Post-operative rat eyes were removed and the corneas were viewed as whole-mounts under a fluorescence microscope to examine the CFDA SE fluorescence. Then the corneas were fixed in formaldehyde and processed for paraffin embedding. Sections of 5 µm were subjected to haematoxylin eosin (HE) staining and observed under a light microscope.

Construction of human corneal endothelium equivalents in vitro: One mm thick, 8 mm diameter APCM lamellae containing Descemet's membrane were prepared and soaked in culture medium at 37 °C for 24 h before cell seeding. They were then placed in a 24-well plate, with the denuded Descemet's membrane facing up. B4G12 cells in 100 µl culture medium were gently seeded at

a density of 1.5×10^5 cells per cm^2 for each scaffold and allowed to adhere for 4 h before being completely immersed in B4G12 culture medium. These were then cultured for 2 wk.

Morphological and histological analysis of corneal endothelium equivalents: The density of the corneal endothelium equivalent was calculated in ten samples after two weeks of organ culture. The surface of corneal endothelium equivalents was stained with trypan blue and alizarin red S. The endothelial side was observed under an inverted microscope. Cell density was determined by counting individual cells in a 0.01 mm^2 area. Three different fields were randomly chosen for each sample. Cell density was expressed as the mean number of cells per $\text{mm}^2 \pm \text{SD}$.

For histological observation, the constructed corneal endothelium equivalents were fixed in 4 per cent paraformaldehyde and processed for paraffin embedding. Five micrometers sections were cut and stained with HE.

Immunofluorescent staining: Fresh corneal endothelium equivalents were embedded in Optimal Cutting Temperature Compound, frozen in liquid nitrogen and stored at -70°C . Primary antibodies were rabbit anti-human ZO-1 Mab (1:20) and mouse anti-human Na^+/K^+ ATPase (1:50). Secondary antibodies were goat anti-rabbit IgG conjugated with FITC (1:100) and goat anti-mouse IgG conjugated with FITC (1:100). Samples were incubated with 10 per cent (wt/wt) goat serum in PBS for 30 min at room temperature before being exposed to primary and secondary antibodies. Samples were incubated with primary antibodies at 4°C overnight and secondary antibodies at 37°C for 30 min. A negligible background was observed for controls (primary antibodies omitted). Cell nuclei were counterstained with DAPI. Fluorescence was observed using an Olympus fluorescence microscope.

Pump function analysis of corneal endothelium equivalents: The pump function of endothelium equivalents was analyzed by corneal swelling assays²⁷. Briefly, the equivalents were mounted in pairs in an in vitro specular microscope. These were perfused with glutathione bicarbonated Ringer's (GBR) solution (6.521 g/l NaCl, 0.358 g/l KCl, 0.115 g/l CaCl_2 , 0.159 g/l MgCl_2 , 0.103 g/l NaH_2PO_4 , 2.454 g/l NaHCO_3 , 0.9 g/l glucose, and 0.92 g/l reduced glutathione). Temperature and pressure were maintained at 37°C and 15 mmHg. After perfusion with GBR for 15 min, the equivalents were switched to calcium-free GBR

for 1 h, to disrupt cell junctions and induce corneal swelling. After 1 h, the equivalents were switched back to either GBR alone for controls or to GBR containing Na^+/K^+ ATPase inhibitor ouabain. Changes in corneal thickness were then measured at various time points with an ultrasound pachymeter. Corneal swelling was reported as the change in equivalents' thickness relative to the initial value for each at the time that ouabain was added. Reported values represent the average of six independent experiments with probabilities calculated using SPSS 17.0 (USA), $P < 0.05$ was considered significant. Fresh porcine corneas and APCM alone were used as normal controls and blank controls, respectively.

Results

Morphology of APCM and B4G12 cells: Histological cross-section confirmed that the major immunogenic porcine corneal keratocytes and endothelial cells were completely removed from the stroma and the Descemet's membrane, and the matrix architecture was well preserved (Fig. 1A).

After 72 h of sub-cultivation, B4G12 cells had formed a dense monolayer of tightly packed cells with polygonal morphology (Fig. 1B), which was similar to native corneal endothelial cells.

MTT assay: MTT assay was used to test the cytotoxicity of APCM. The results showed that the mean OD values of the experimental group on day 1, 3, 5, 7 were 0.646, 1.114, 1.215, 1.258, respectively, having no statistical differences ($P > 0.05$) with those of the control group at each corresponding point 0.66, 1.122, 1.221 and 1.295. This meant that there was little residual toxic SDS in thoroughly-washed APCMs and the proliferation of B4G12 cells was not influenced (data not shown).

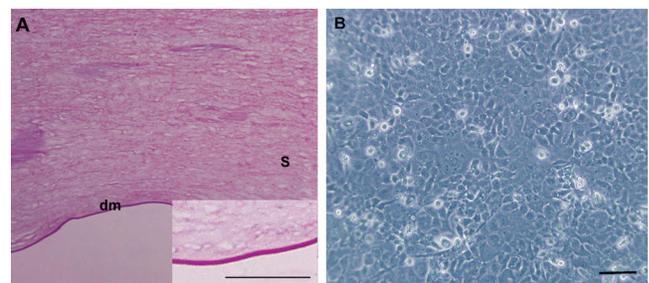


Fig. 1. Microscopic images of APCM and B4G12 cells. (A) HE staining showed that the acellular porcine corneal matrix was cell-free and the collagen structure was preserved. A high magnification image of APCM is shown in the lower right corner. (B) Monolayer of B4G12 cells formed after 72 h of sub-cultivation. Scale bars: A=50 μm , B=100 μm . dm= Descemet's membrane; s= stroma.

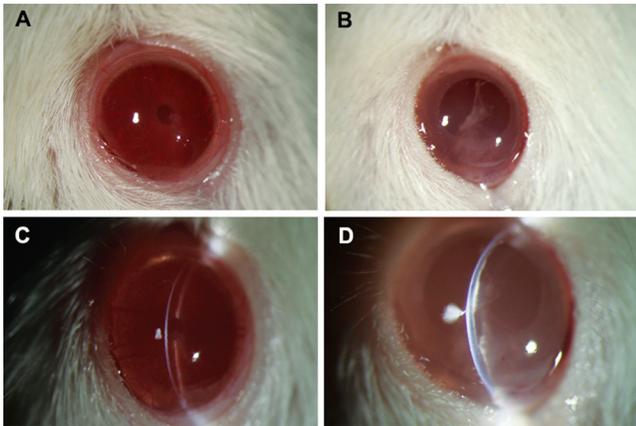


Fig. 2. Representative corneal photos after the surgery. **(A)** Cornea in the B4G12 cell-injection group was clear, the anterior chamber and the iris were clearly visible. **(B)** In contrast, cornea in the cryoinjury only group was opaque. **(C)** The slit image of the cornea in the B4G12 cell-injection group showed that the cornea was at normal thickness, and the endothelium surface was smooth. **(D)** The slit image of the cornea in the cryoinjury only group showed that the cornea was swollen and there was lamellar keratic precipitate on Descemet's membrane.

Bio-safety and function analysis of B4G12 cells in vivo: B4G12 cells were labelled with CFDA SE according to the manufacture's instruction before the surgery. Representative photographs of the anterior segment showed that corneas in B4G12 cells-injection group were clear with the anterior chamber clearly visible, while in the cryoinjury only group the corneas were opaque with stromal edema (Fig. 2A and B). The slit images showed clearly that the corneas in the cryoinjury only group were about twice the thickness of those in B4G12 cells-injection group one month after surgery (Fig. 2C and D).

HE staining showed a monolayer of cells on Descemet's membrane in the B4G12 cell-injection group, whereas no cells could be seen on Descemet's membrane in the cryoinjury only group (Fig. 3A and B). A fluorescence signal was detected in corneal flat mounts in the B4G12 cell-injection group, indicating that their origin was from B4G12 cells not host corneal endothelial cells (Fig. 3C). There was no evidence of mononuclear cell accumulation or neoplasm from B4G12 cells around Descemet's membrane, suggesting no immunological reaction or oncogenicity of B4G12 cells in this model.

Characterization of constructed corneal endothelium equivalents: The human corneal endothelium equivalents were efficiently constructed with B4G12 cells and APCM. The initial seeding density (1.5×10^5

cells/cm²) assured that the cells formed a monolayer which had covered the Descemet's membrane of APCM after 2 wk (Fig. 4A). Staining of cell nuclei (DAPI staining) also indicated that cells were only present on Descemet's membrane and that the scaffold was free of keratocytes in the stroma (Fig. 4B).

Dual staining of corneal endothelium with trypan blue and alizarin red S is widely used for delineation of living corneal endothelial cells. As shown in Fig. 4C, the result revealed complete cell coverage. Most B4G12 cells stayed alive after being cultured on APCM and the dye-lake reaction showed a clear outline of the margins of B4G12 cells. The mean cell density of 10 corneal endothelium equivalents was 2061 ± 344 cells/mm² (range 1389 to 2689 cells/mm², n=30)

Immunofluorescent localization of ZO-1, a tight-junction associated protein, was used to check whether the cells formed a closed monolayer. The result revealed that this protein accumulated at cell boundaries, suggesting that B4G12 cells could form a closed monolayer on APCM (Fig. 5A and a). The primary role of corneal endothelium is to keep the relative dehydration state of cornea stroma, so the presence of

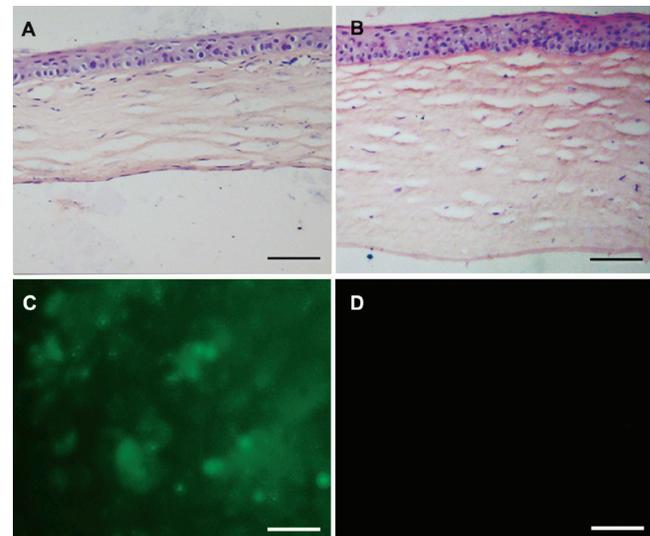


Fig. 3. Histological examination of the corneas after the surgery. **(A)** HE-stained cross-section showed that Descemet's membrane was covered by cell monolayer in the B4G12 cell-injection group. **(B)** No cells were present on Descemet's membrane in the cryoinjury only group. Note that the corneal stroma was much thicker than that in the B4G12 cell-injection group. **(C)** Fluorescence microscopy confirmed that cells covering the Descemet's membrane in the B4G12 cell-injection group were CFDA SE-positive. **(D)** No signal was detected from the corneas of the cryoinjury only group. Scale bars: 100 μ m.

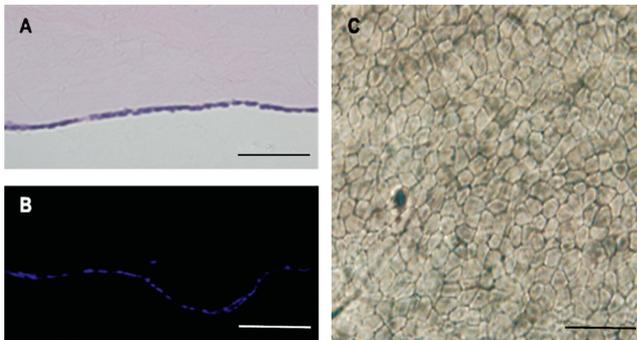


Fig. 4. Histological analysis of the corneal endothelium equivalents. **(A)** HE staining showed there was a monolayer of cells covering the Descemet's membrane of the APCM. **(B)** DAPI staining confirmed the cell coverage of the Descemet's membrane of the APCM. **(C)** Trypan blue and alizarin red S co-staining showed the B4G12 cells were alive and clearly delineated the cell boundaries. Scale bars: 50 μm .

Na^+/K^+ ATPase, a protein complex responsible for the pumping function was also detected. A positive signal was detected between cell nuclei (Fig. 5B and b). These two proteins were expressed in a similar pattern to native B4G12 cells on their natural substrate.

Having confirmed expression of Na^+/K^+ ATPase in constructed human corneal endothelium equivalents, corneal swelling assay was performed to determine the pump function. Changes of corneal thickness were compared with fresh porcine corneas denuded of epithelium. Calcium-free GBR solution transiently caused corneal swelling and then it was switched back to GBR with or without Na^+/K^+ ATPase inhibitor ouabain. As shown in Fig. 6, calcium-free GBR solution initialized corneal swelling after 20 min perfusion. The corneal equivalents continued to swell after GBR solution was switched back for both of equivalent

group and equivalent-ouabain group, but the corneas swelled to a much greater degree in the latter group. The average increase of the corneal thickness in the equivalent group after 100 min was 63 versus 89 μm for that of the equivalent-ouabain group, and the difference was statistically significant ($P < 0.05$). The result showed that treatment with ouabain dramatically affected corneal thickness of the equivalents that were constructed. This changing pattern was similar to that of fresh porcine corneas denuded of epithelium. In contrast, APCM alone kept swelling when incubated in GBR solution both in the presence of calcium or ouabain. These findings indicated that the B4G12 cells formed a monolayer having CEC-like pump function on APCM with adequate transport activity.

Discussion

Corneal organ culture serves as a useful model that allows research to be done under conditions that are relatively similar to the *in vivo* state without being interfered with by the ocular surface barrier and the blood-aqueous humour barrier. But due to the lack of donor corneas and limited proliferative capacity of CECs, corneal organ culture is mostly limited to corneal epithelial research.

Tissue-engineering technology now provides a new opportunity by constructing artificial corneal endothelium equivalents for *ex vivo* studies and potential clinical use. The construction of tissue-engineered corneal endothelium involves two major elements: seed cells and scaffold. The great advantage of human corneal endothelial cell line is the easy accessibility compared to primary CECs. Human CECs are in the post-mitotic state *in vivo*, which

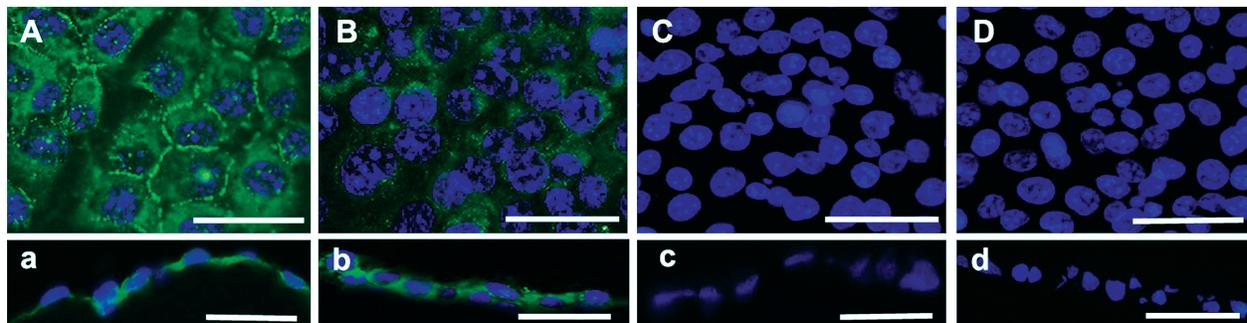


Fig. 5. Immunofluorescent determination for ZO-1 and Na^+/K^+ ATPase. **(A and a)** ZO-1 was mainly expressed at the cell borders of corneal endothelium equivalents. **(B and b)** Na^+/K^+ ATPase was detected in the cell plasma and membrane of corneal endothelium equivalents. **(C and c)** Negative control in which the primary antibody was omitted for ZO-1. **(D and d)** Negative control in which the primary antibody was omitted for Na^+/K^+ ATPase. A, B, C and D are plane views of corneal endothelium equivalents and a, b, c and d are corresponding cross-section views. Scale bars: 50 μm .

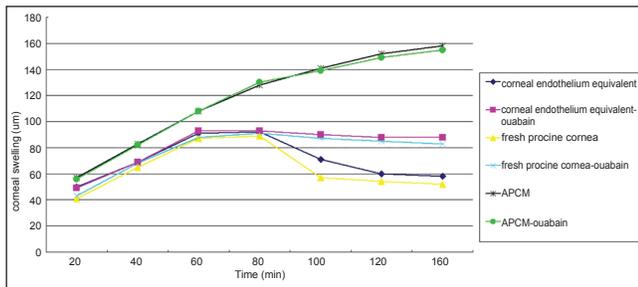


Fig. 6. Pump function analysis of corneal endothelium equivalents by corneal swelling assay. Changes of corneal thickness were compared with fresh porcine corneas denuded of epithelium and APCM itself. Each value is the mean change of corneal thickness \pm SD. Calcium-free GBR solution could induce corneal swelling in fresh cornea group, APCM group and corneal endothelium equivalent group. When it was switched back to normal GBR solution, the corneal swelling regressed in both of fresh cornea and corneal endothelium equivalent group, but not in APCM group. Addition of ouabain to GBR solution dramatically inhibited the regression of corneal swelling in fresh cornea and corneal endothelium equivalent group by interfering with the pump-function of Na^+/K^+ ATPase.

makes studies of cultured endothelial cells *in vitro* a big challenge. The human corneal endothelial cell line was first constructed in 2000⁵, and two clonal cell lines B4G12 and H9C1 were separated from this cell population in 2008²². This B4G12 cell line was chosen as a substitute for primary human CECs because it was found to have the features very close to primary human CECs and could serve as a good model^{22,23}. Another merit of this cell line is that it is cultured in a serum-free medium. The cornea is an avascular organ, which is not physically in contact with serum. But according to the common protocol, primary CECs need to be cultured under a serum-containing condition²⁸. The impact of serum on cell morphology or even cell physiology is hard to predict, which may affect the reliability of the results, especially for toxicological screening of drugs and investigation of pathological corneal endothelium conditions. Thus, a serum-free system is necessary for corneal endothelium organ culture^{29,30}.

The similarity in function to native cells and bio-safety have always been critical in choosing candidate seed cells for artificial organ construction. Thus *in vivo* B4G12 cells transplantation was conducted to see if these were appropriate candidate cells. Our results demonstrated that B4G12 cells behaved well without causing an immunological reaction or showing their oncogenicity in our rat model.

Various tissue-engineered corneal endothelia have been constructed using different scaffolds. The

APCM scaffold used in this study proved to be free of native cell components and similar to natural corneal stroma regarding transparency, biocompatibility and mechanical strength as shown in our previous reports¹⁹⁻²¹. In this study, it was shown that APCM could support the growth of B4G12 cells and expression of the tight junction protein ZO-1 and functional pump protein Na^+/K^+ ATPase. It was noticed that some sections of the constructed corneal endothelium equivalents were multilayered, which was probably due to cell clumps generated during the seeding procedure. Filters with the proper size could help to get rid of the clumps in order to get a strictly monolayer endothelium. A few groups have conducted vital pump function detection of their tissue-engineered corneal endothelia^{18, 31-33}. The results of the corneal swelling assay in this study not only demonstrated that the constructed corneal endothelium equivalents had the pump function *in vitro*, but also further proved that the collagen structure of the APCM was preserved after the decellularization process and the hydration was reversible, just as in the natural cornea.

In conclusion, our study demonstrated that APCM combined with B4G12 could make corneal endothelium equivalents similar to native corneal endothelium in both morphology and function, which might serve as good models of corneal endothelium organ culture for *ex vivo* studies.

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